A Better Bladder for ECMO Controls Pump Flow as a Function of Inlet Pressure

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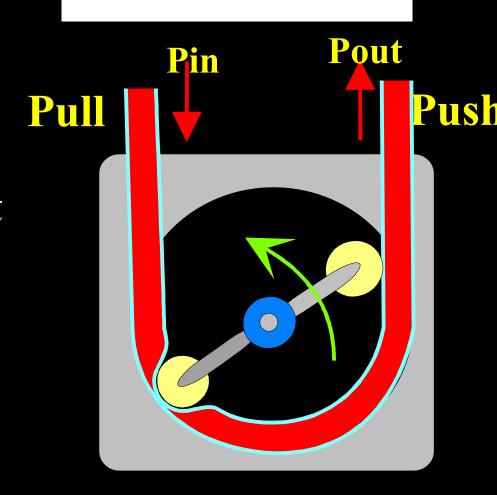
Supported by NIH NHLBI Grant # R44HL-46057

The most popular pump used for ECMO is the roller pump. The RP is a positive displacement pump that is insensitive to inlet or outlet pressure.

The pump can generate:

- Pin -600 mmHg
- Pout > 2,000 mmHg



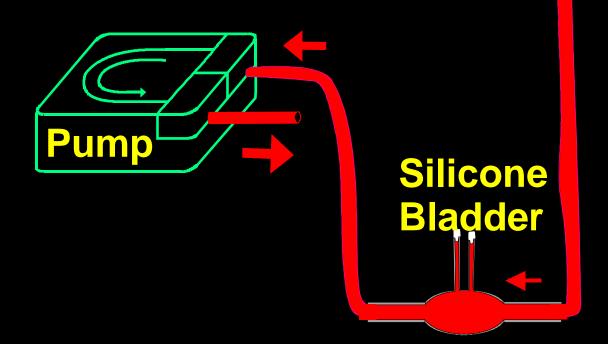


What does the Bladder do?

Patient

The Bladder protects the patient from the excess negative pressure the pump can generate

and that can damage the blood as well as the cannulated blood vessel.

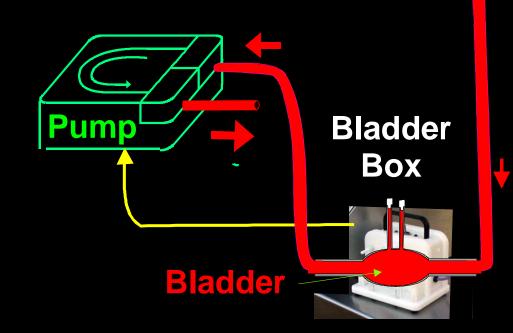


How does the Bladder/Bladder Box Work?

When inlet pressure to the pump falls below ambient pressure, the silicone bladder empties. A microswitch senses an empty bladder and switches off the power to the pump.

Patient

When the bladder refills the pump restarts.

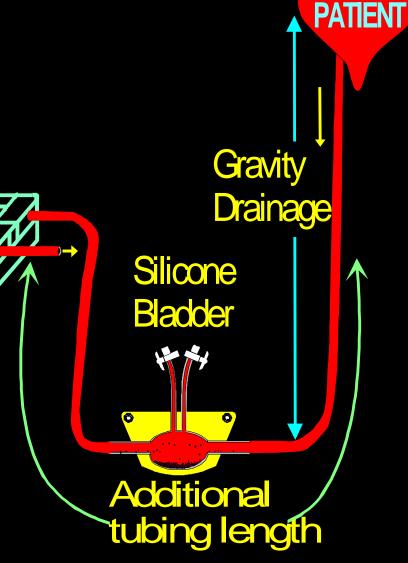


Silicone Bladder/Bladder Box Limitations

Flow Control

Gravity DrainageDependent = Bladderon Floor

On - Off Flow Control

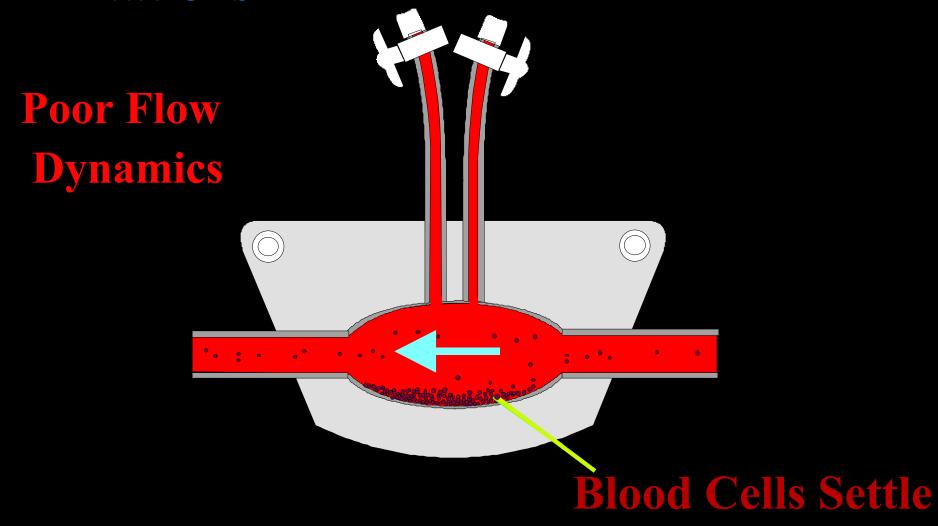


Silicone Bladder + Bladder Box Limitations

Long Tubing (Patient to Floor)

- Greater prime volume
- Larger foreign surface
- Blood resides in tubing for a longer time (greater heat loss and greater blood/surface interaction)

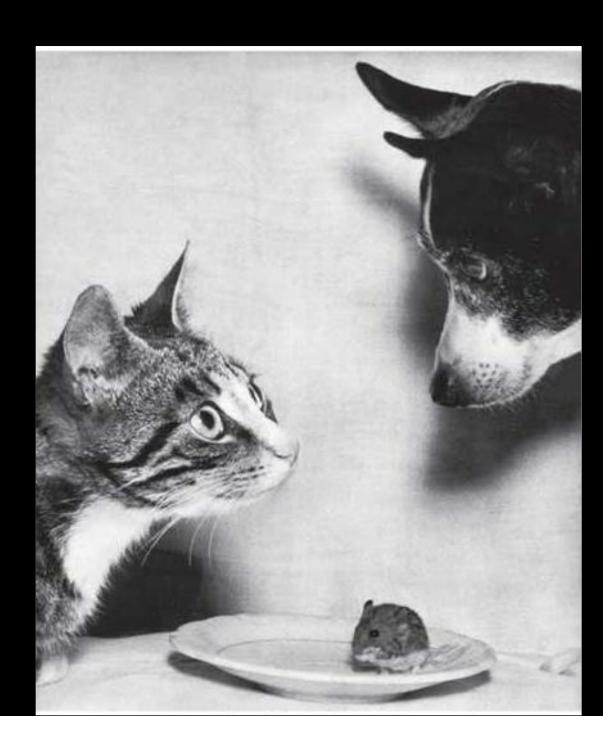
Silicone Bladder + Bladder Box Limitations



Limitations of the Silicone Bladder, Summary

- 1. Maximum flow is limited to the height of the patient above the floor
- 2. On/Off control does not takes advantage of computer controlled roller pumps
- 3. Poor flow dynamics more prone to clotting.
- 4. Placement on the floor can be hazardous
- 5. Difficult to use when transporting a patient

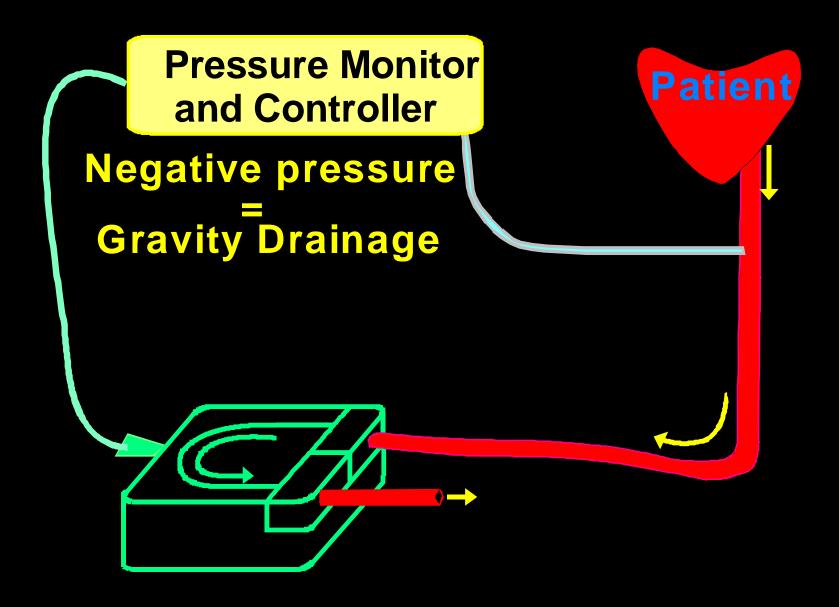
What to do?



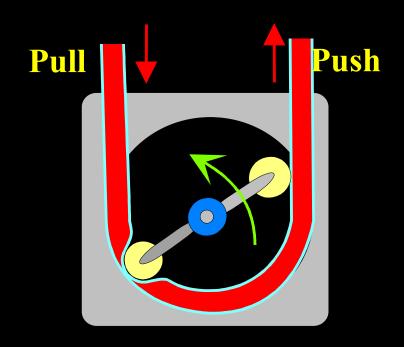
Develop a Better-Bladder System that provides:

- VAVD for roller pumps that increases flow
- On/Off or Continuous flow control
- Flow pattern less conducive to cell settling
- Shorter tubing
- Need not be placed on the floor

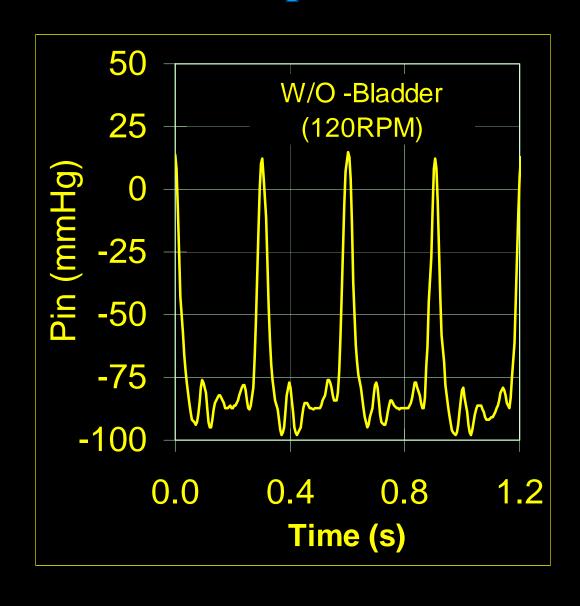
Control pump speed as a function of inlet pressure



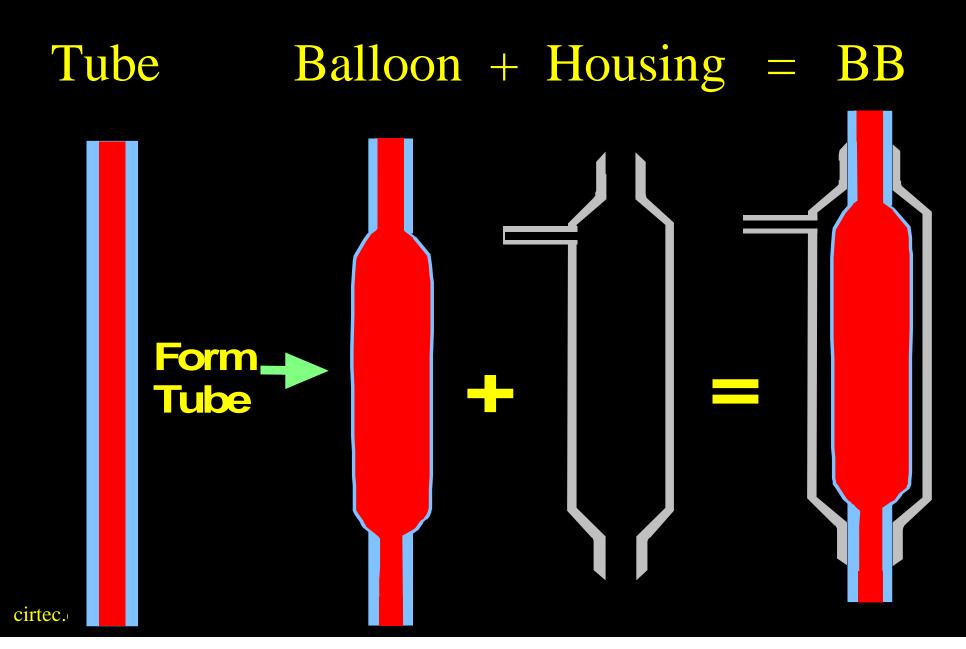
The Inlet Pressure of a Roller Pump is Pulsatile



Pulsatile pressure at pump inlet prevents smooth pump control

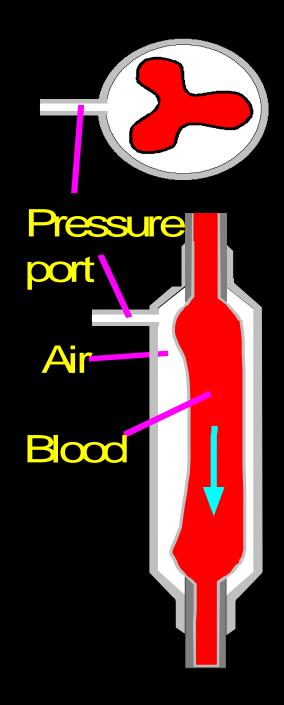


How the Better-BladderTM is Made

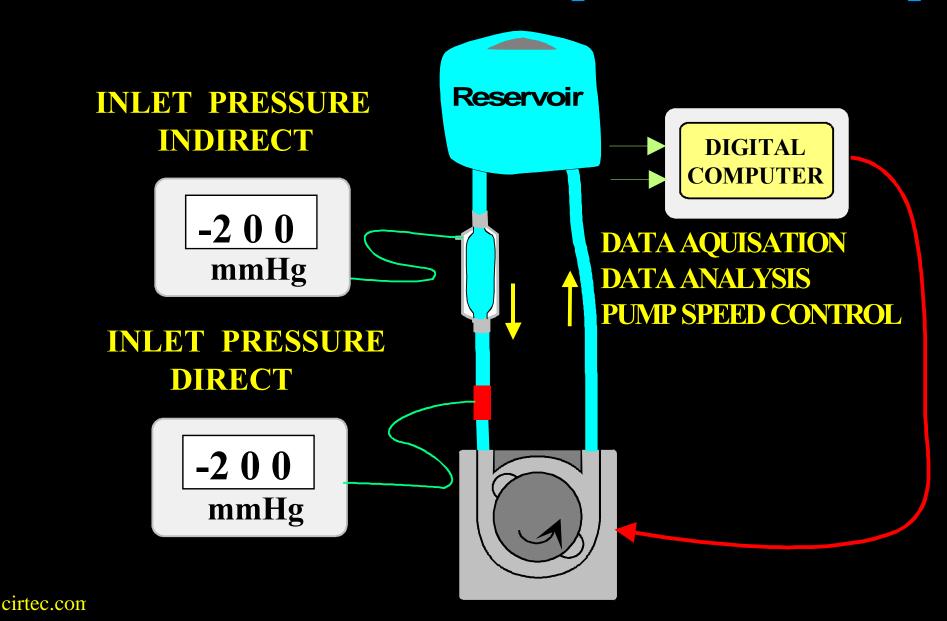


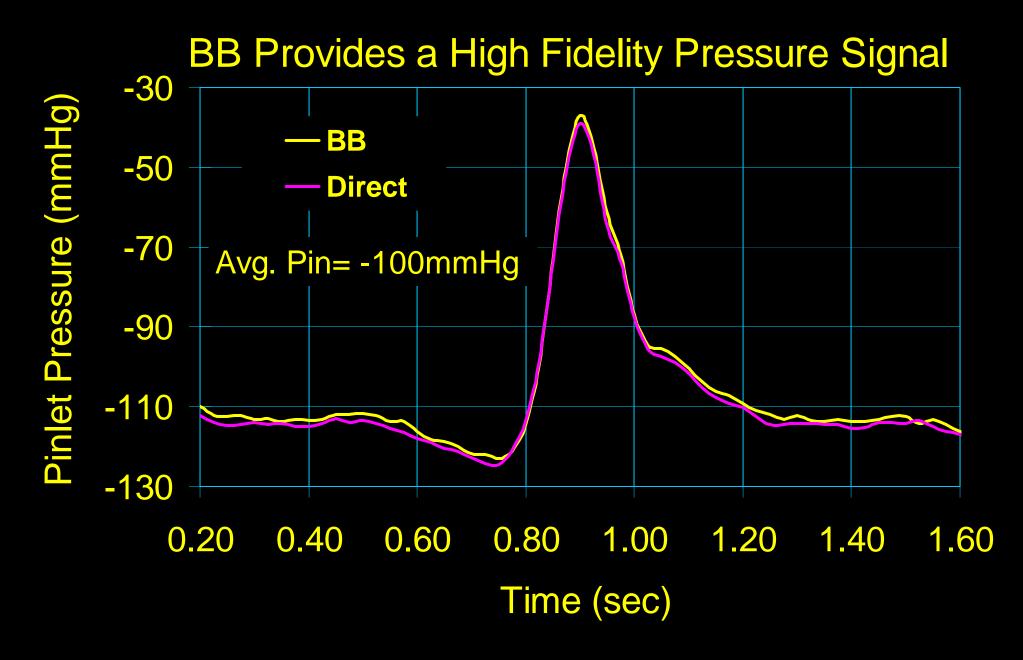
The Better-Bladder

- Senses Pressure
- Provides Compliance

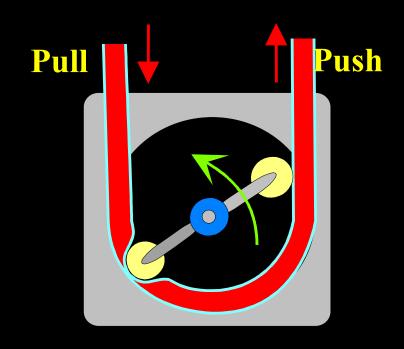


Functional Tests: Experimental Setup

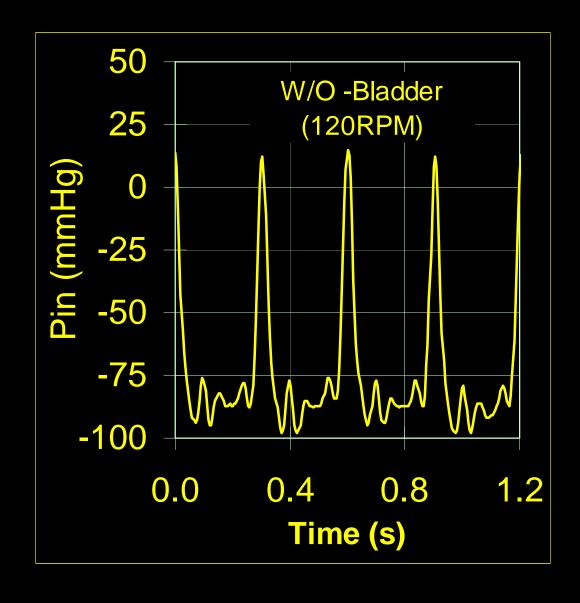




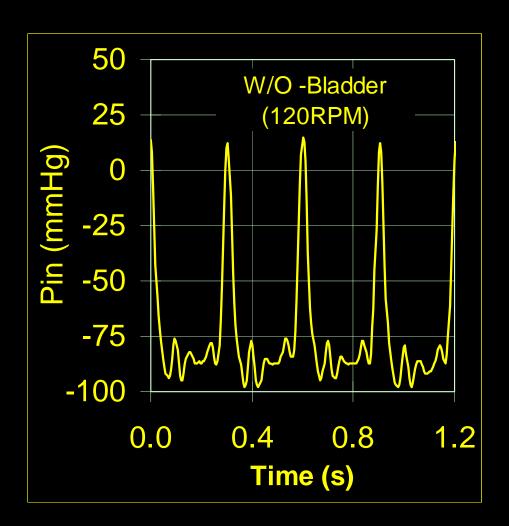
The Inlet Pressure of a Roller Pump is Pulsatile

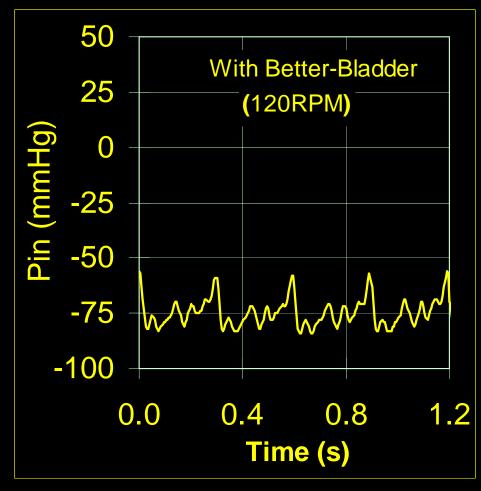


Pulsatile pressure at pump inlet prevents smooth pump control



Roller Pump + BB Inlet Pulse Pressure is Dampened



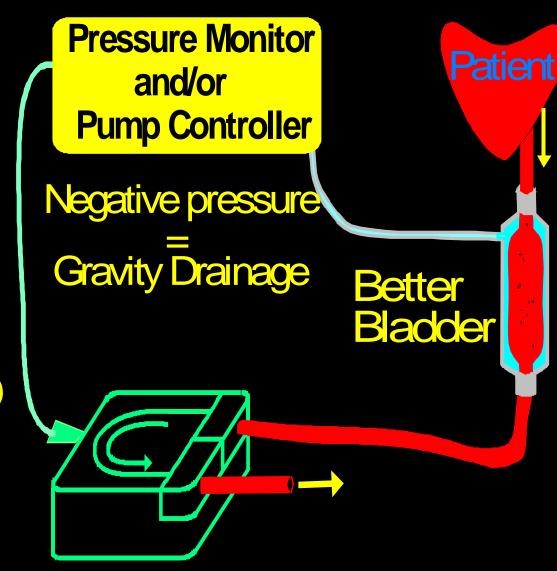


Pump Control with the Better-Bladder:

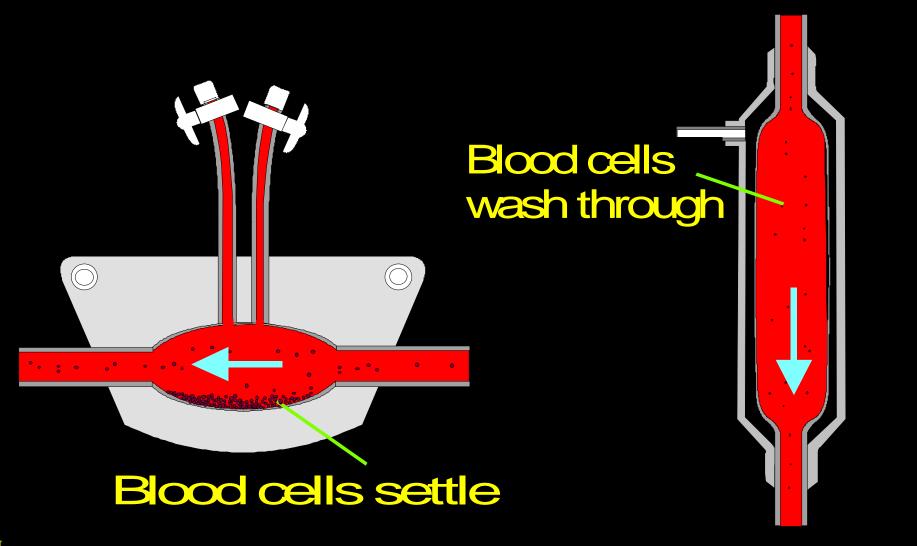
Inlet pressure signal controls pump speed:

On/Offor

Continuos (e.g. CAPS)



Better Flow Dynamics Silicone Bladder Better-BladderTM

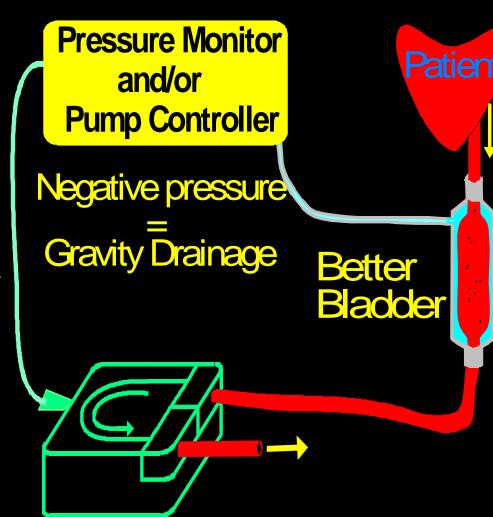


The BB Allows Increased Flow

Flow = $\Delta P/Resistance$

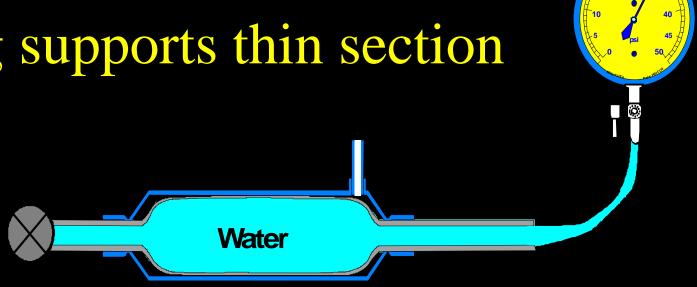
The older bladder collapsed at ambient pressure. The BB collapses at the negative pressure set by the user. Blood can be actively pulled from the patient.

No need to raise the bed or drop the bladder to the floor.

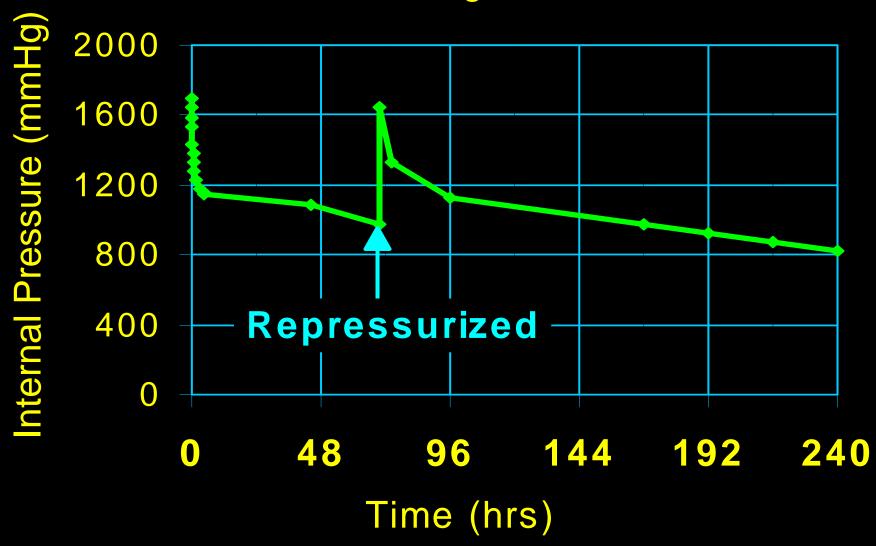


High Pressure Tests of Balloon

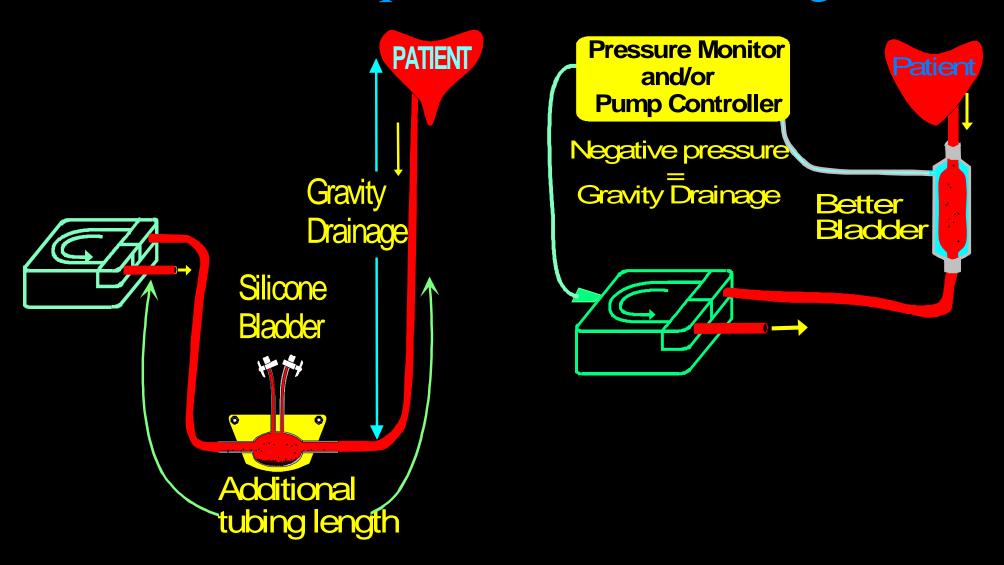
- Housing side is open to atmosphere
- 1500 mmHg applied to blood side
- Balloon expands to housing
- Housing supports thin section



The BB Withstands Large Internal Pressures

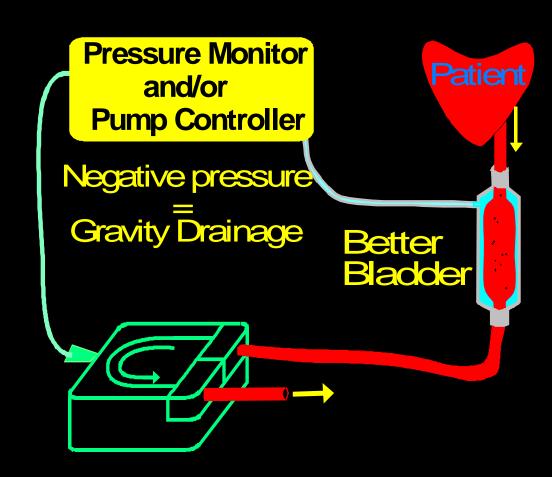


The BB Requires Shorter Tubing



The Better-Bladder Provides:

- "Adjustable" gravity drainage - VAVD
- Flow less conducive to cell settling
- On/off or continuous flow control (e.g. CAPS system)
- Shorter circuit tubing



The Better-Bladder Provides

Shorter Tubing

- Lower prime volume
- Reduced foreign surface
- Blood resides in tubing for a shorter time (lowers heat loss and blood/surface interaction)

510(k) Number K98-1284
Device Name Better-BladderTM

http://www.accessdata.fda.gov/scripts/cdrh/cfdocs/cfPMN/pmn.cfm

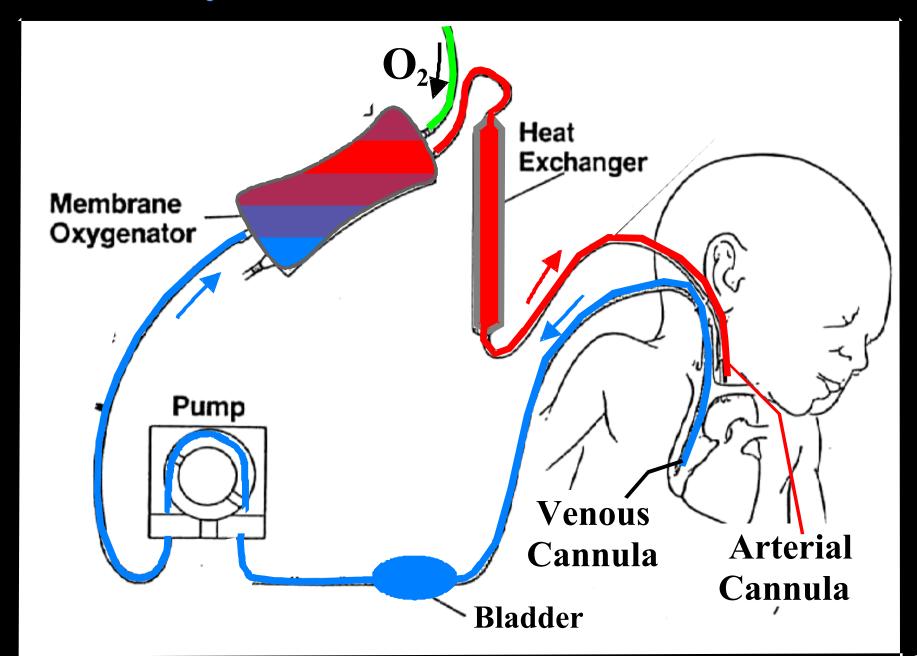
Indications for Use – The Better-BladderTM is a device that isolates pressure transducers form blood contact when measurements of blood pressure in extracorporeal circuits are made during short and *long term* procedures. The pressure signal can be used to control pump speed. It is also used as an inline reservoir to provide compliance in the circuit during short and *long term* term procedures.

To Bladder or not to Bladder?

Yehuda Tamari

Circulatory Technology Inc. Oyster Bay, NY

Why use a Bladder for ECMO?

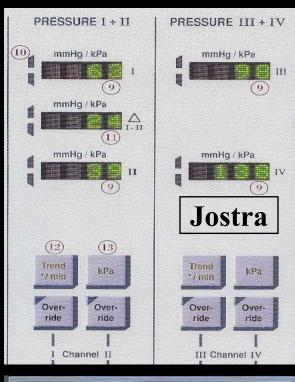


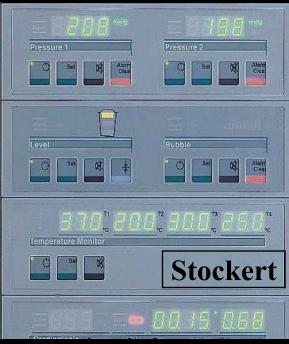
Computerized Roller Pumps

Blood flow is controlled as a function pump inlet pressure.

When inlet pressure drops below a settable pressure the pump slows down or stops.

When inlet pressure increases above the set point, pump flow returns to its set value.





Recent comments/questions from the ECLS-Net

- "Is anyone removing or considering removing the bladder out of their ECMO circuit that uses roller pumps?"
- "We have PVC tubing in place of the bladder and it has worked very well."
- "We have a collapsible Silastic bridge."

No reasons were given for eliminating the bladder.

Cost? Complexity? reliability?

There were no mentions of using a bladder with centrifugal pumps.

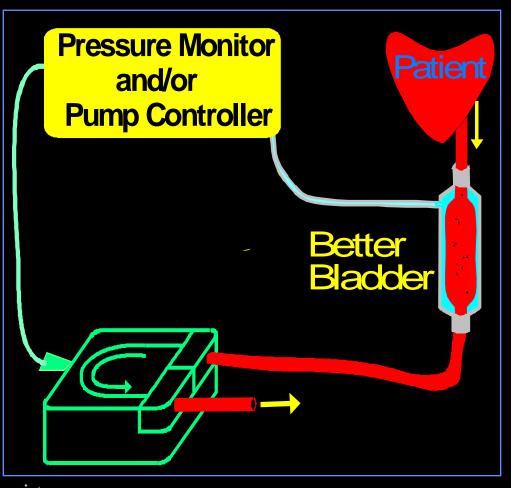
When making changes to a circuit

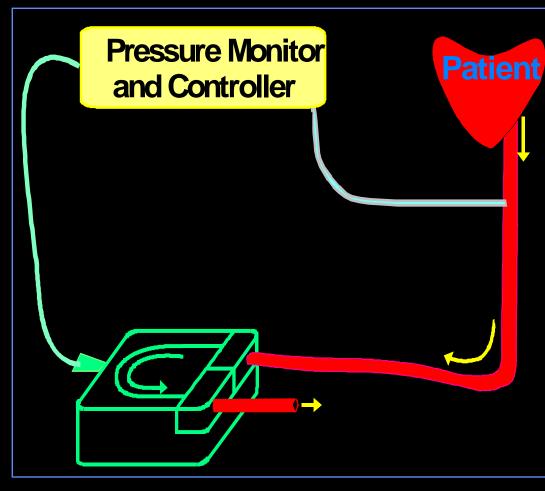
Practice Caution

- What follows are results of some tests that we conducted with and without a bladder under ECMO settings.
- Serve as an outline for the type of tests that should be conducted prior to removing or replacing the bladder.

Pump flow is controlled as a function of inlet pressure Should we pump

with a bladder or without a bladder





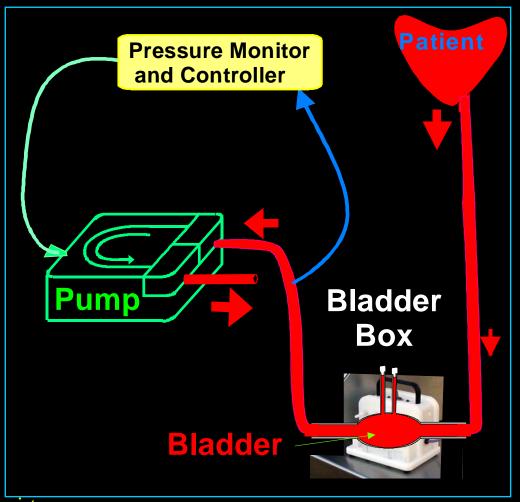
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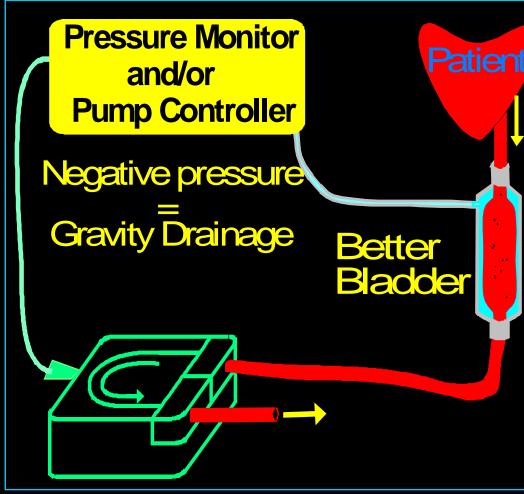
Pump flow is controlled as a function of inlet pressure

Compliance can be provided by

The Silicone Bladder

The Better Bladder





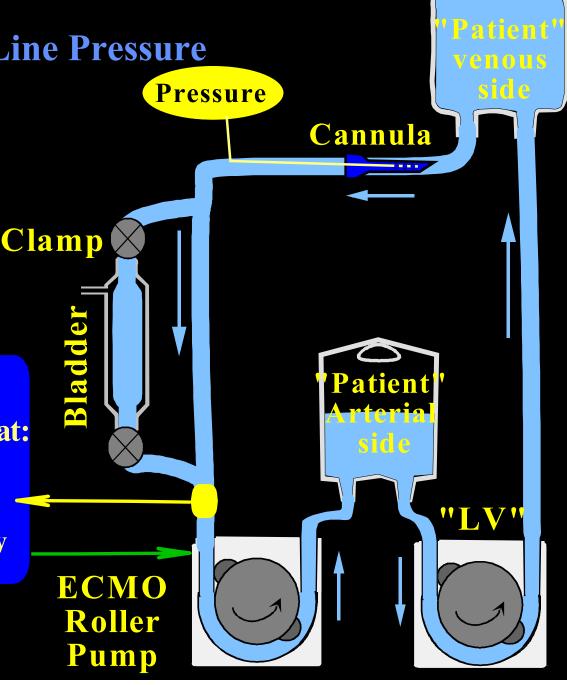
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Experimental Setup Pump Controlled by Venous Line Pressure

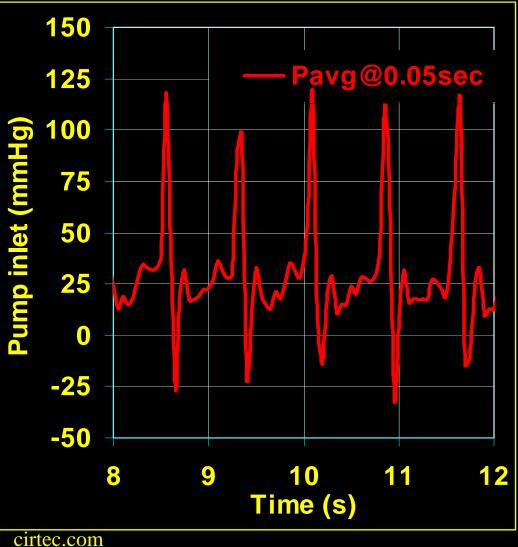
Controller set to stop flow at Pin = -30mmHg
Reduce venous flow below pump flow and record the pressures

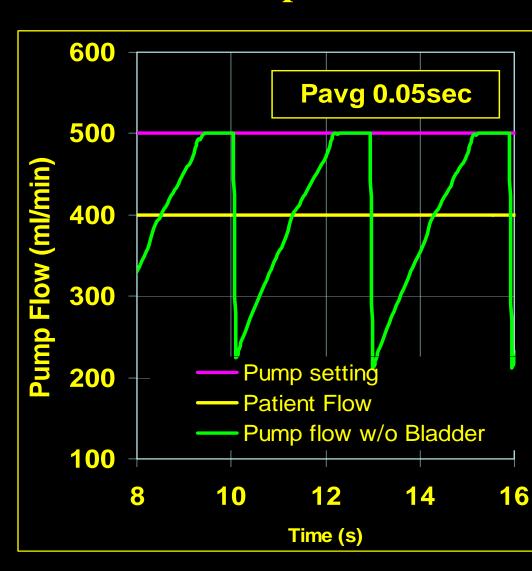
Sample rate-1000/sec

Data Acquisition
Measure pressure at:
Cannula tip
Pump inlet
Control Pump flow



Pump Controlled by the Instantaneous Inlet Pressure: w/o a Bladder Results in Erratic Pump Flow



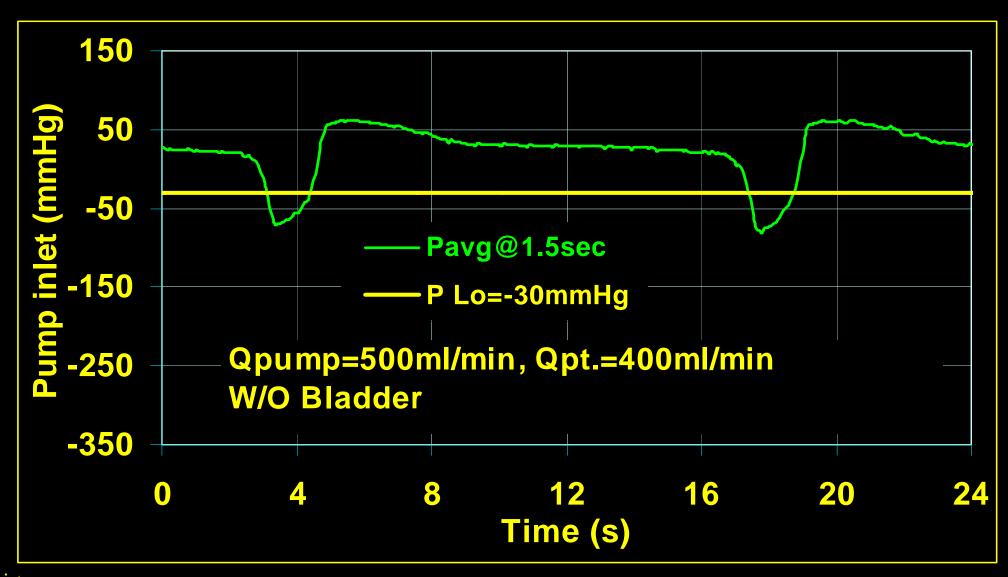


Pump Controlled by the Instantaneous Inlet Pressure: Electronic Pressure Averaging



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Pump Controlled by Electronically Averaged Inlet Pressure

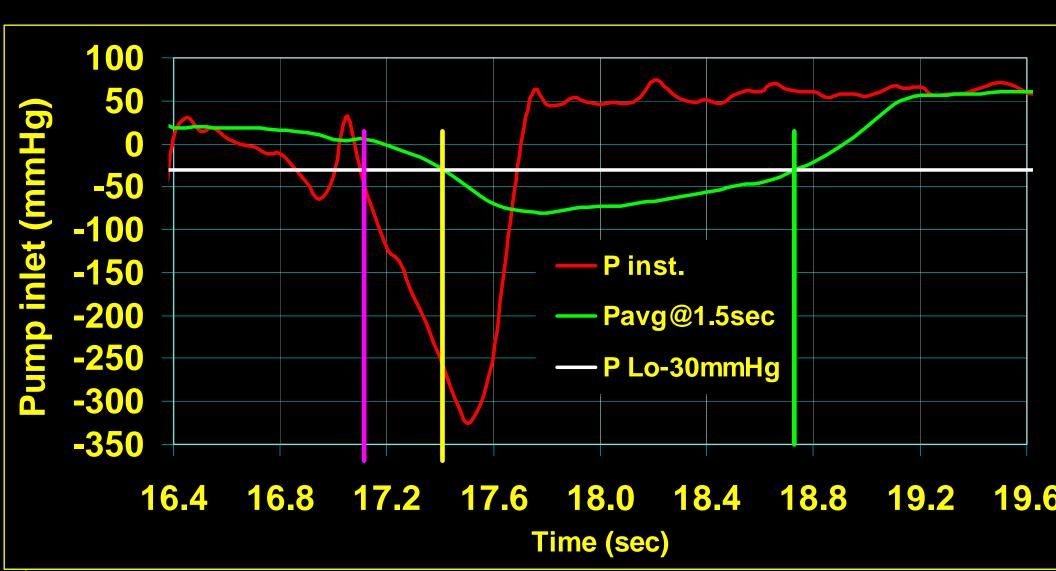


Pump Controlled by Electronically Averaged Inlet Pressure



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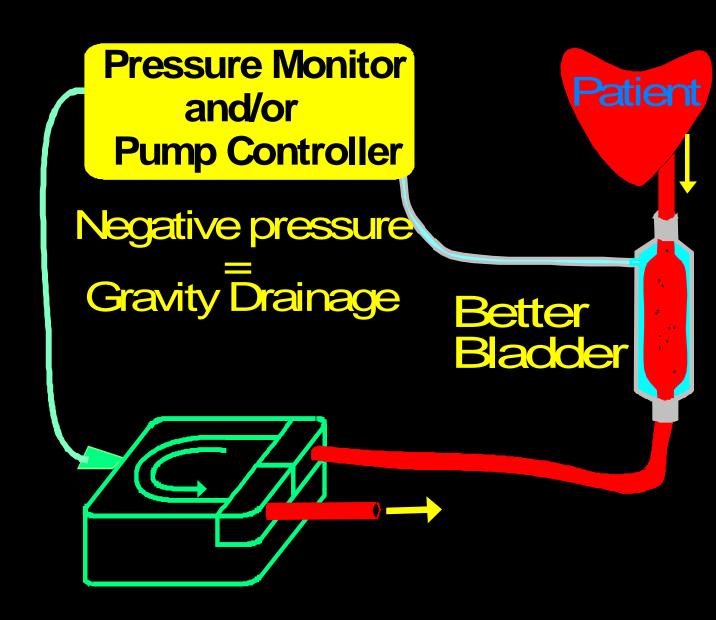
Pump Controlled by Electronically Averaged Inlet Pressure w/o a Bladder



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The BB at the Pump Inlet
Provides
compliance
and reduces
pressure

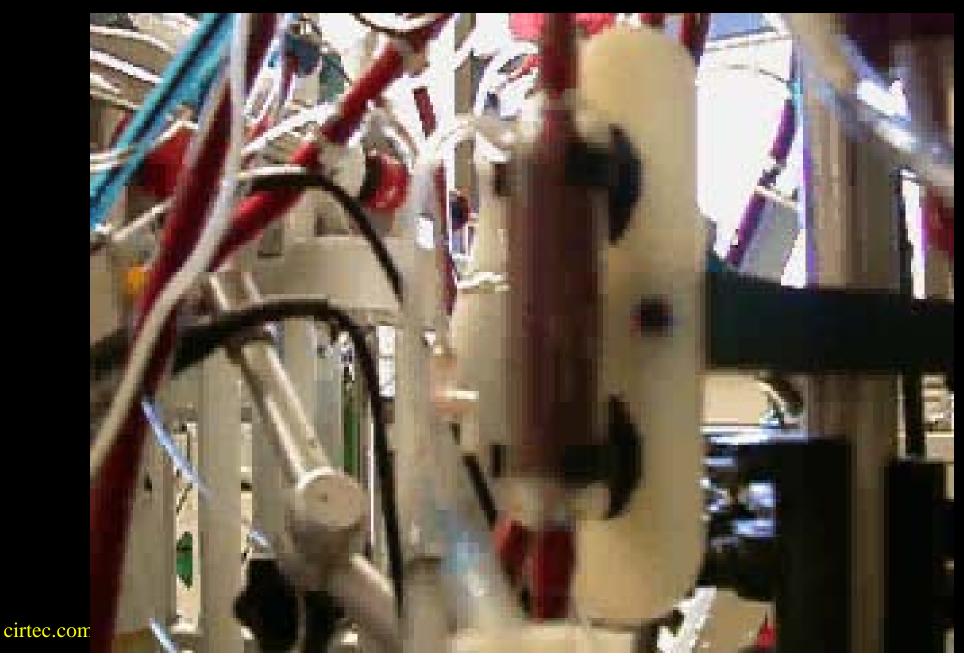
pulsation.



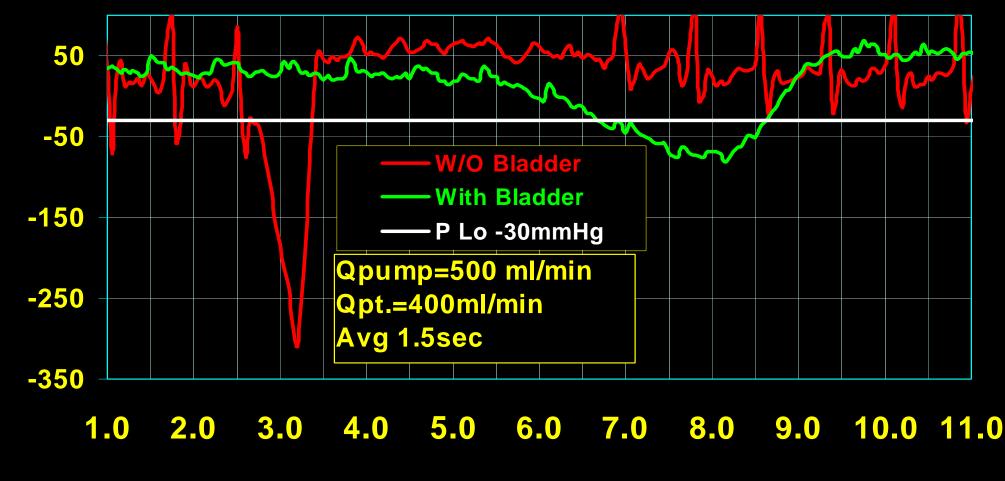
Roller Pump with a Bladder at its Inlet



Bladders Absorb the Pressure Fluctuations of the Roller Pump



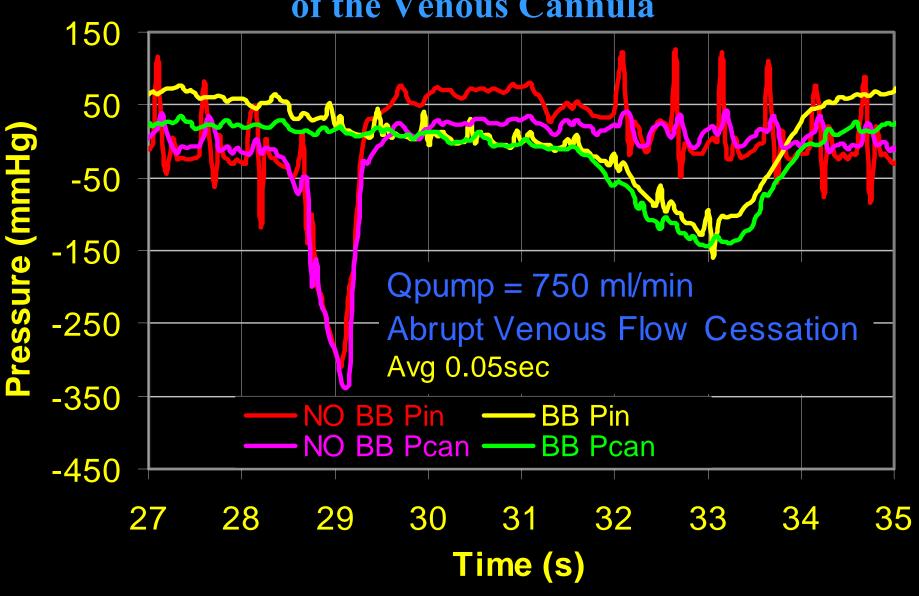
Pump Controlled by Electronically Averaged Inlet Pressure With a Bladder



Time (sec)

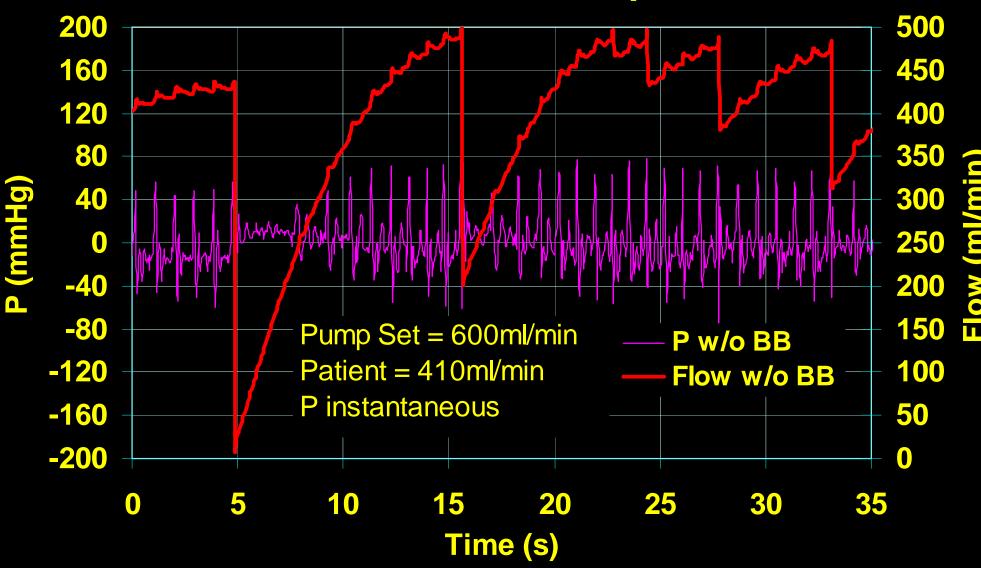
Pump inlet (mmHg)

High Negative Pump Inlet Pressure is also Seen at the Tip of the Venous Cannula

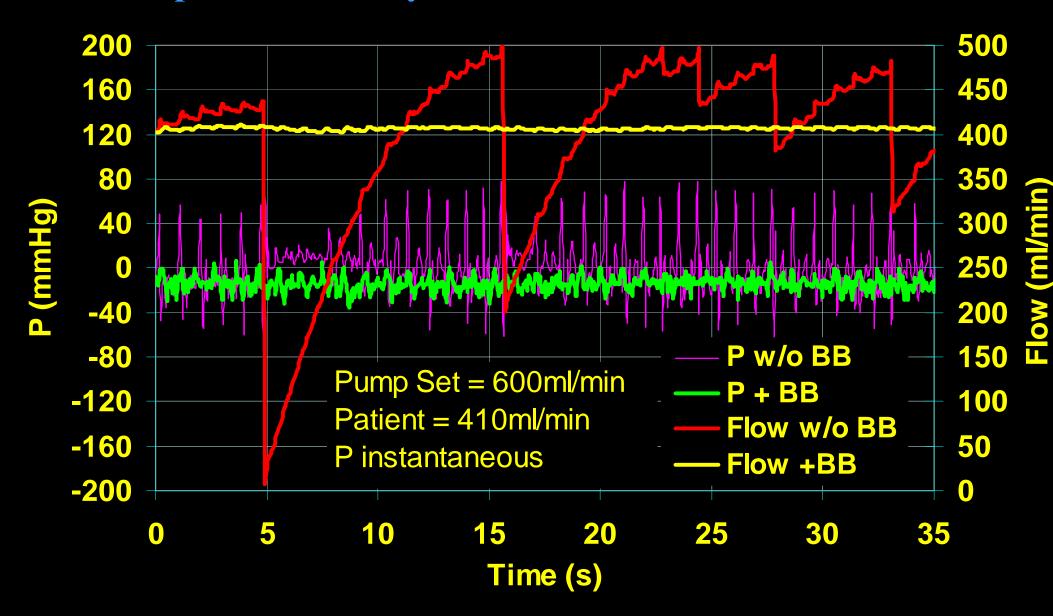


Pump Controlled by the Instantaneous Inlet Pressure:

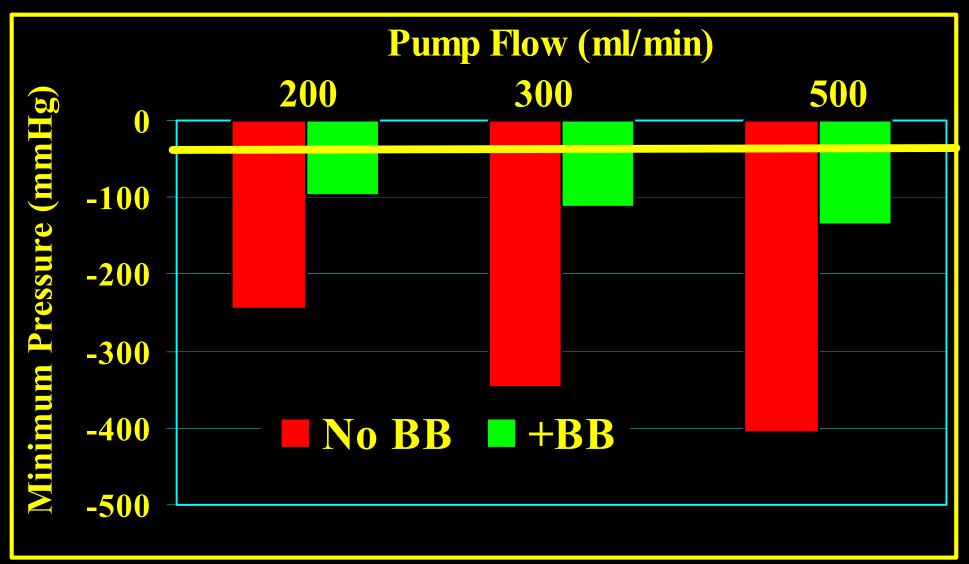
Results in Erratic Pump Flow



Pump Controlled by the Instantaneous Inlet Pressure



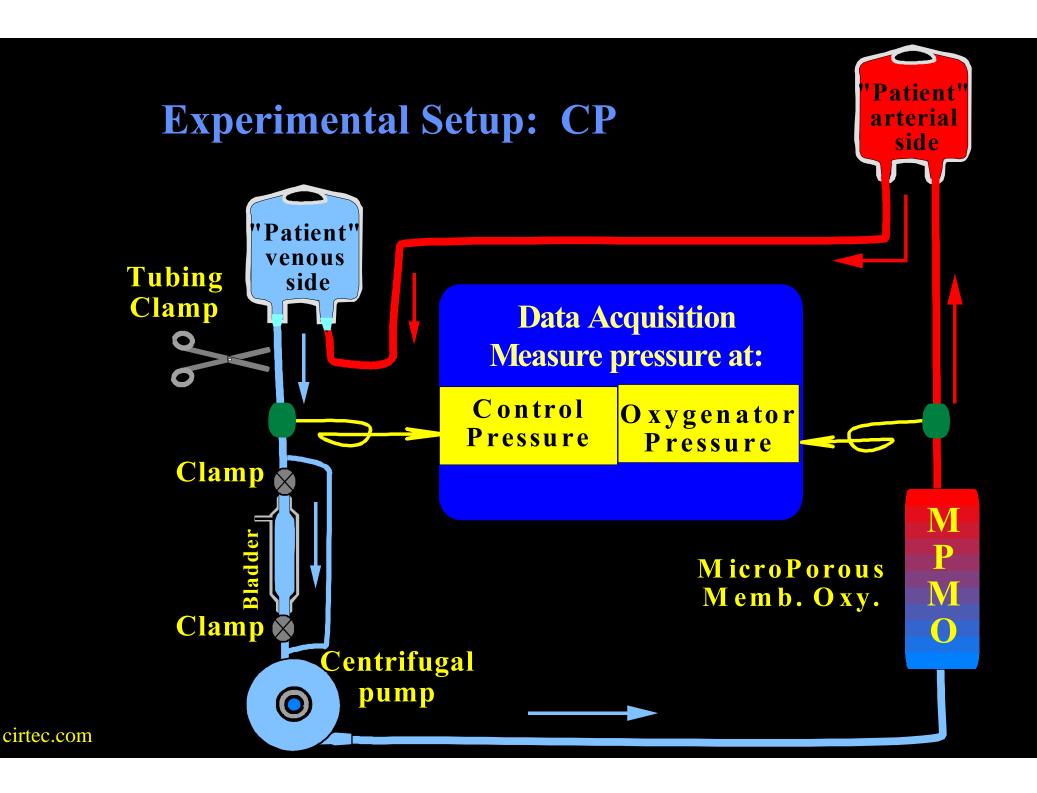
Maximum Suction due to Abrupt Stoppage of Venous Flow. Using the Jostra roller pump with and w/o a bladder



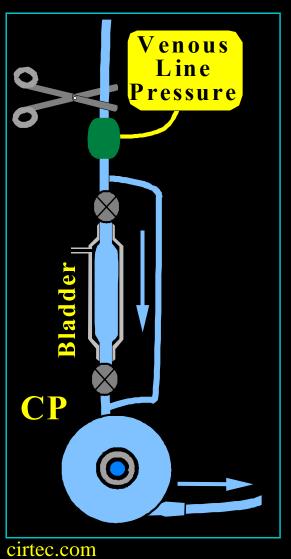
Are Bladders Required When Centrifugal Pump are Used for ECMO?

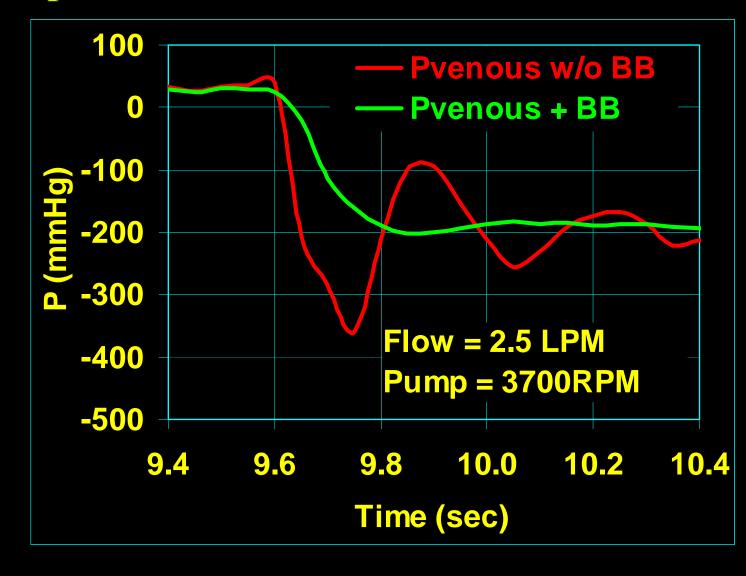
Effects of a bladder placed at the pump inlet on:

- the maximum negative pressure at pump inlet due to abrupt stoppage of venous flow.
- the pump outlet pressure due to abrupt stoppage of venous flow.
- the air handling of a CP.

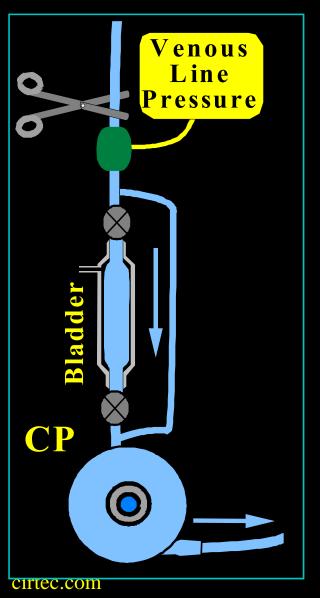


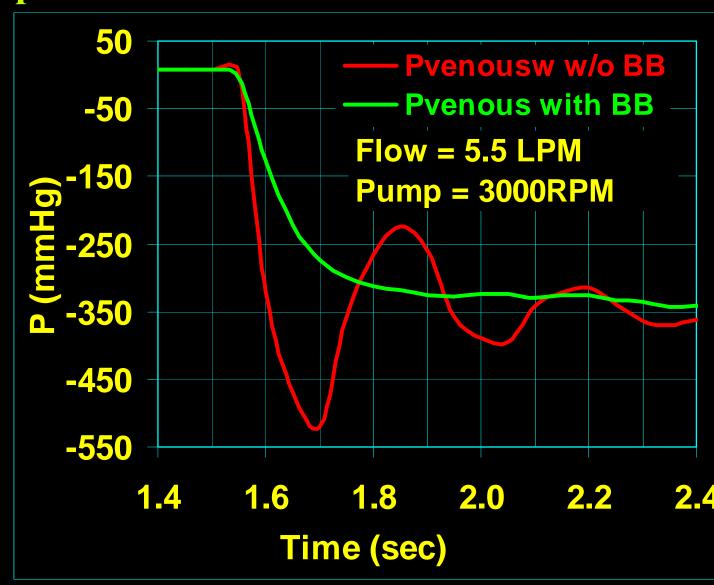
Inlet Pressure to a CP - Abrupt blockage of Venous Flow Pressure drops faster and lower w/o a bladder



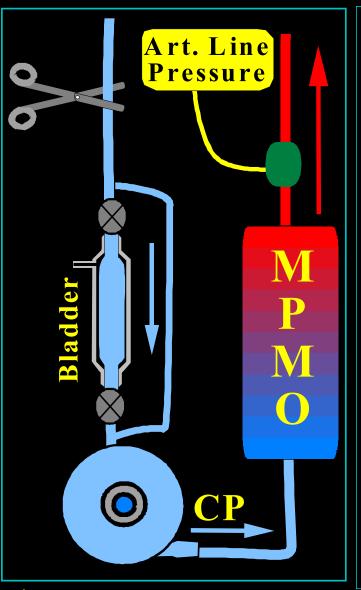


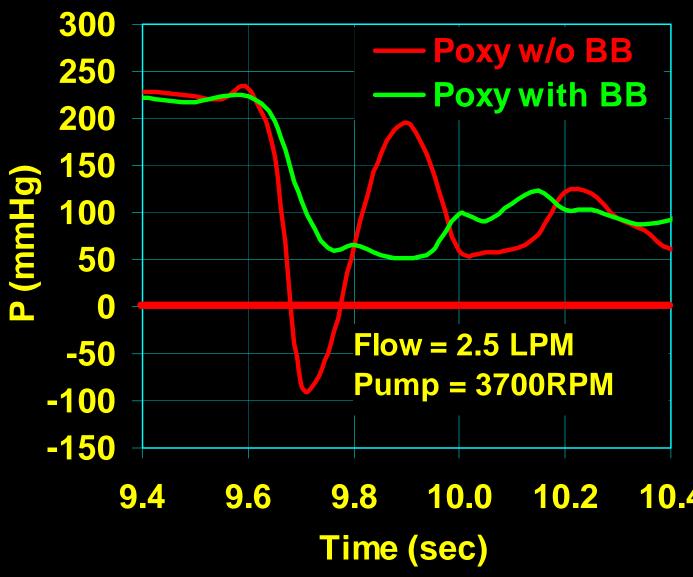
Inlet Pressure to a CP - Abrupt Blockage of Venous Flow Pressure drops faster and lower w/o a bladder





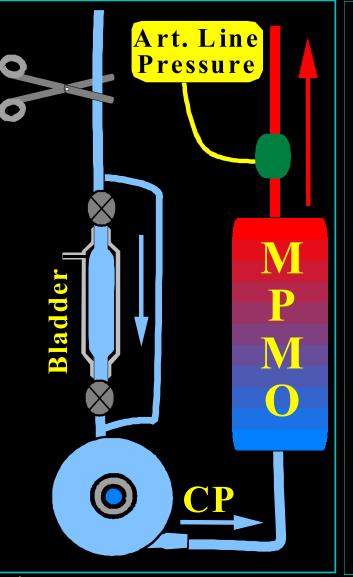
Pressure at Oxygenator can Become NEGATIVE

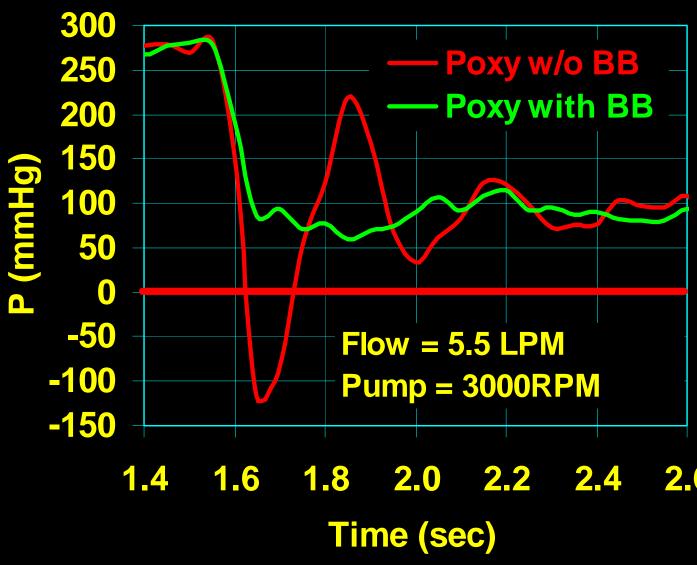




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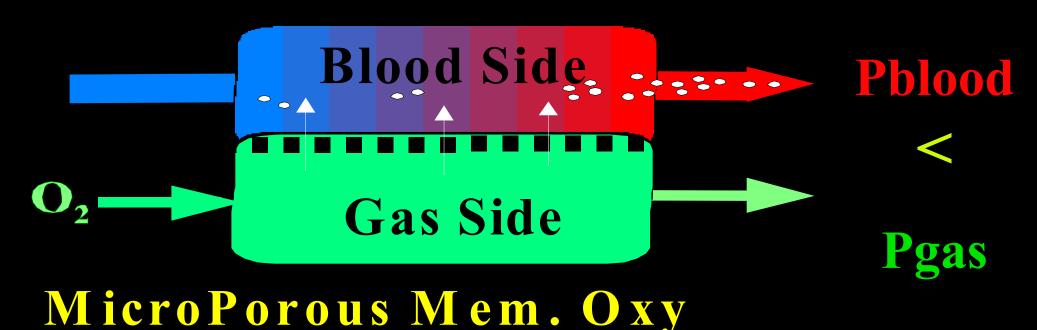
Abrupt stoppage of Venous Flow can Cause the Pressure at Oxygenator to go **NEGATIVE**

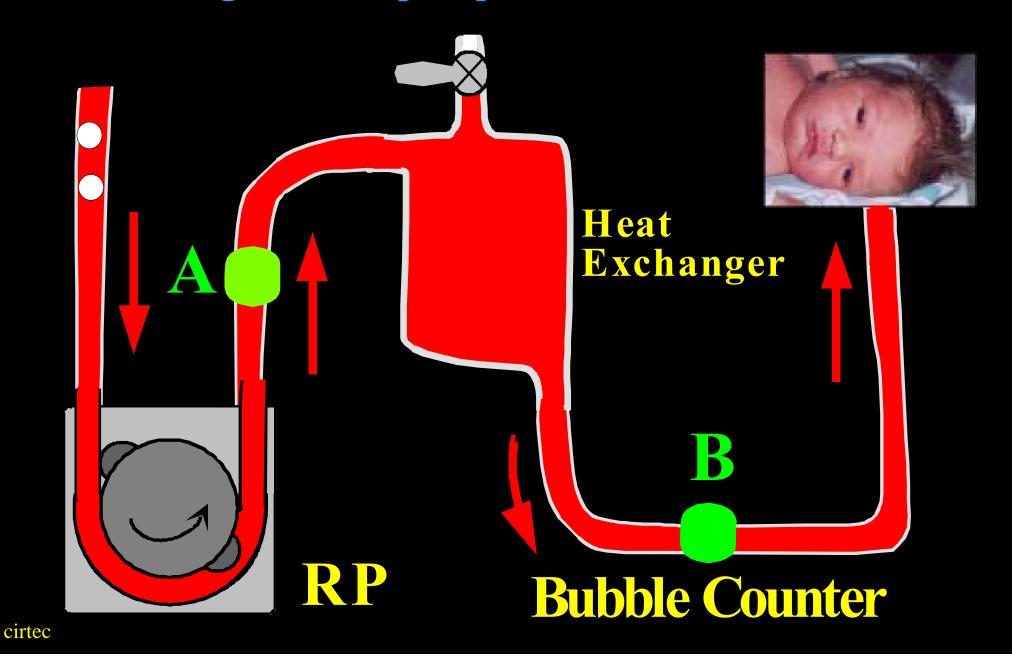


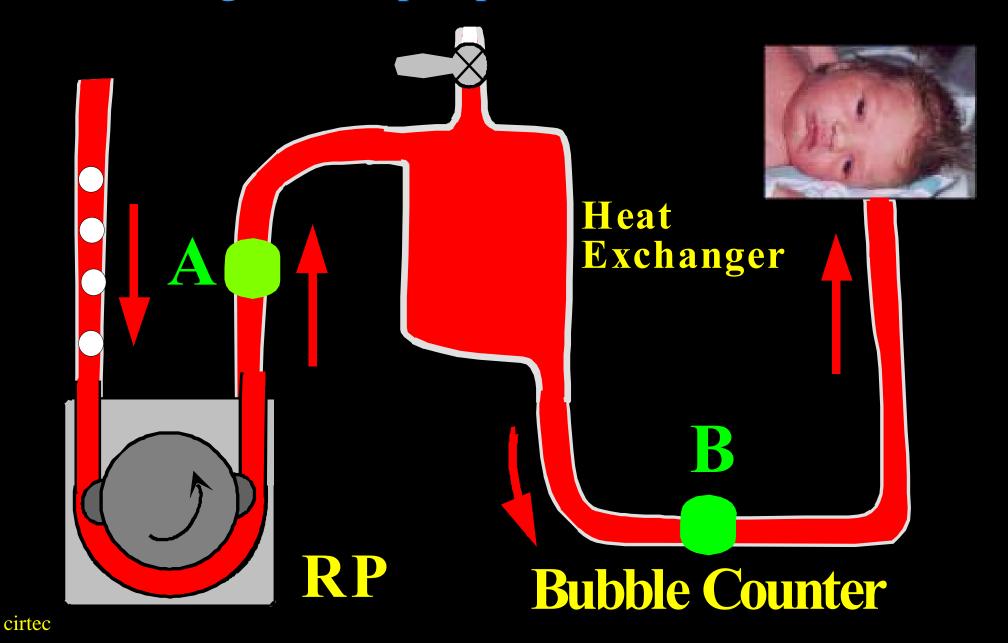


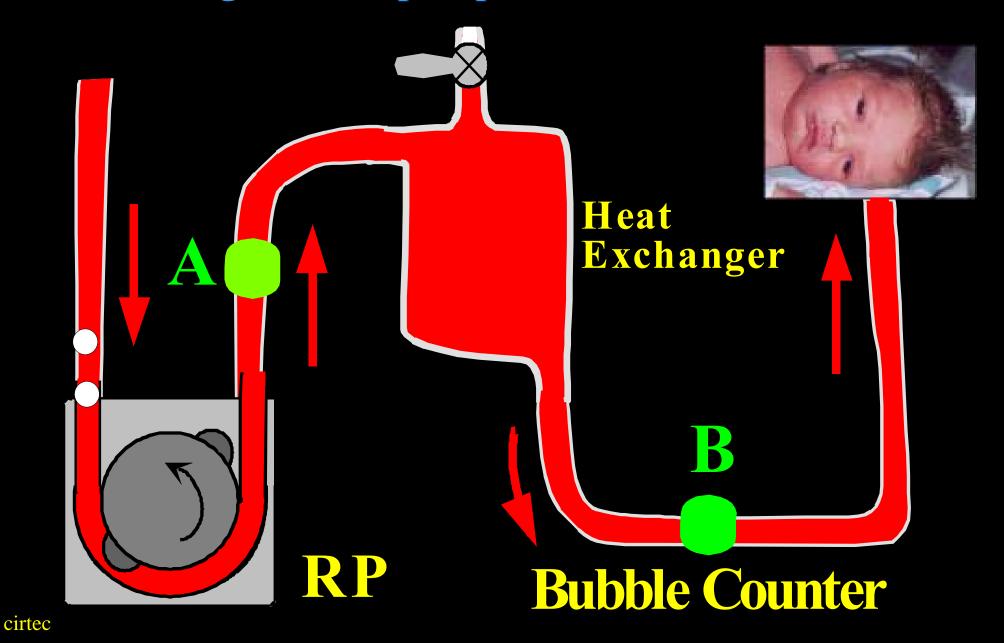
Abrupt stoppage of Venous Flow can Cause the Pressure at Oxygenator can Become NEGATIVE

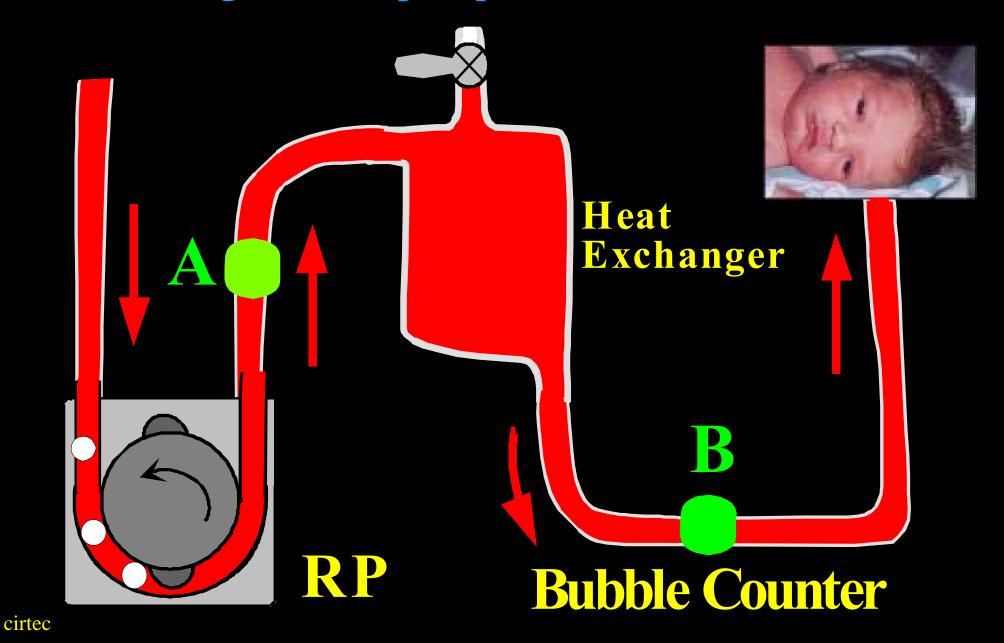
When pressure on blood side of a MPMO falls below the gas pressure then there is a significant possibility that gas will flow across the porous membrane into the blood side of the oxygenator and into the arterial line.

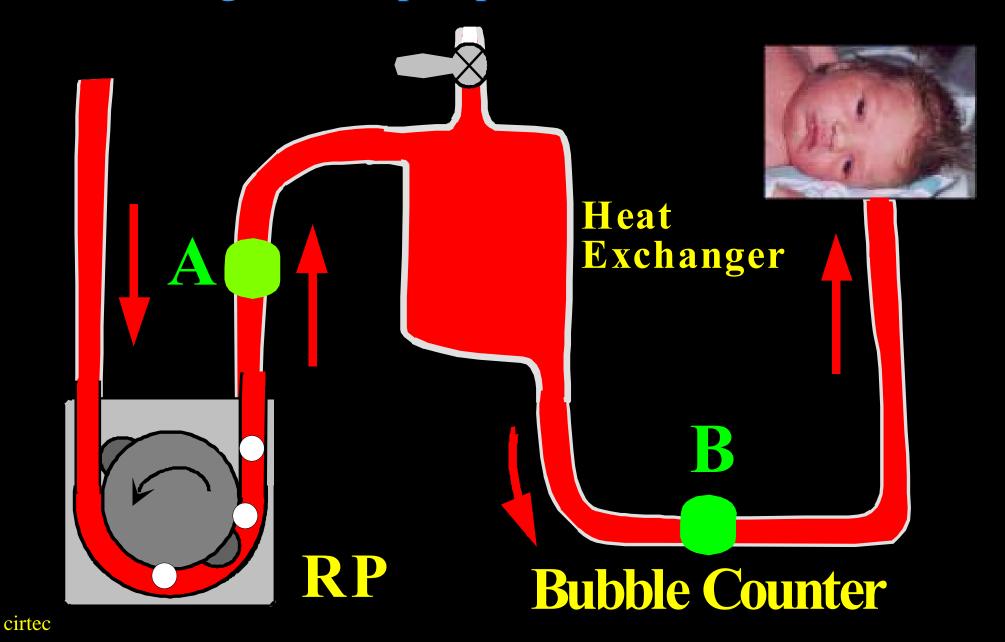


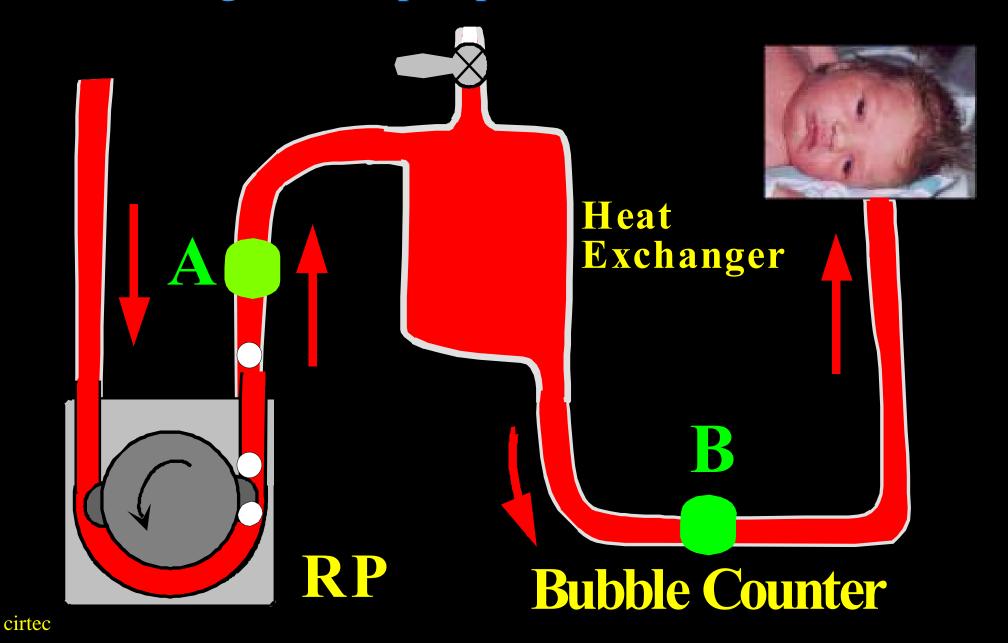


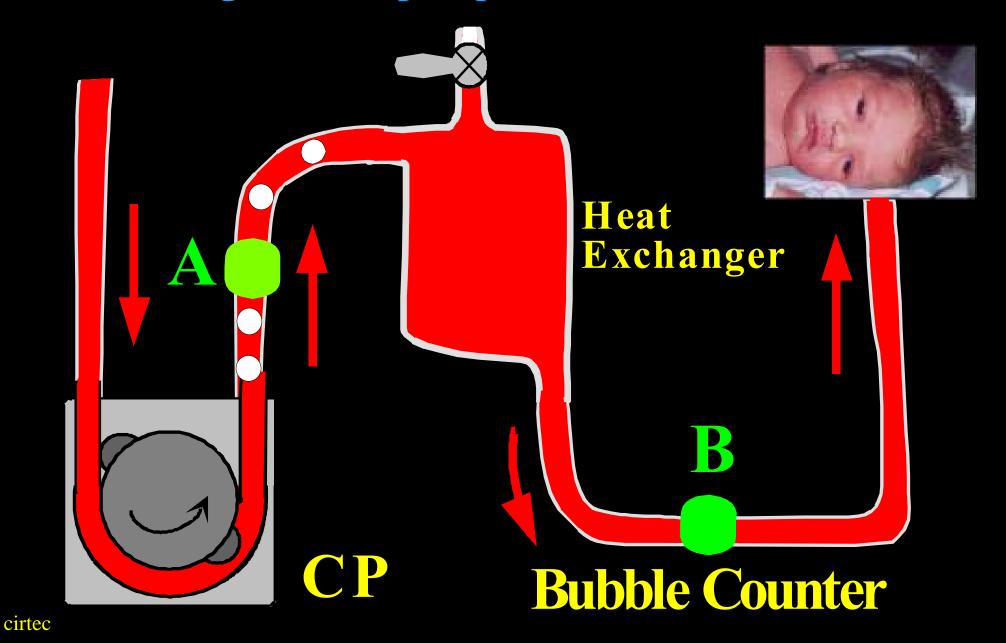


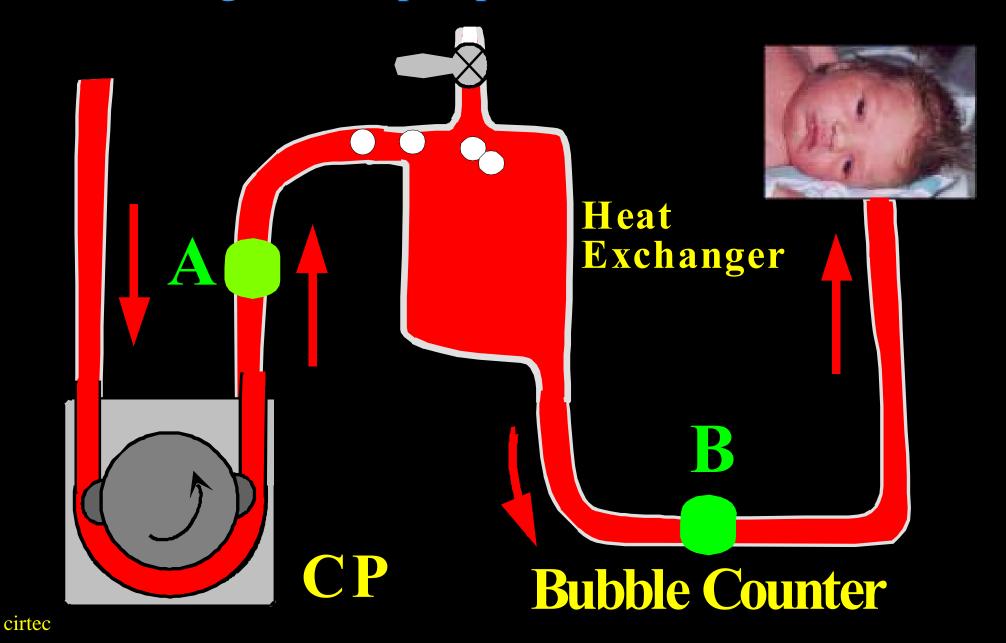


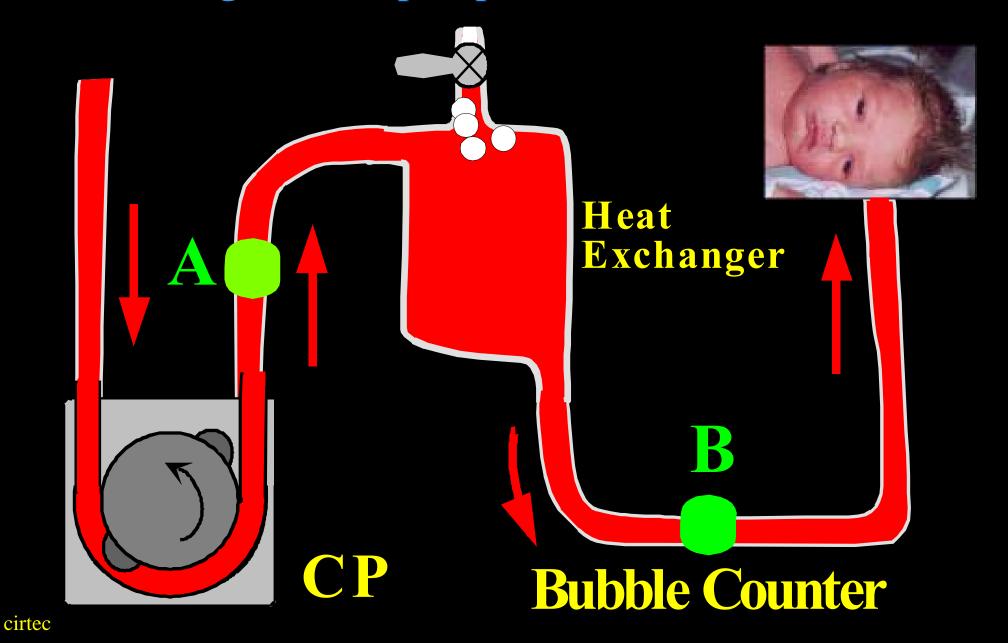


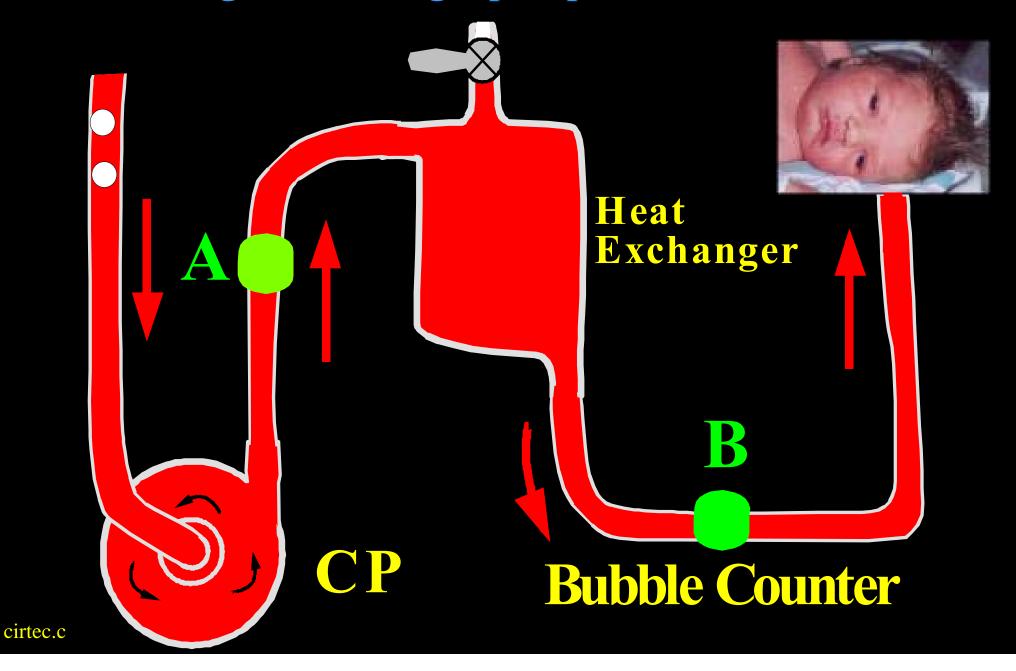


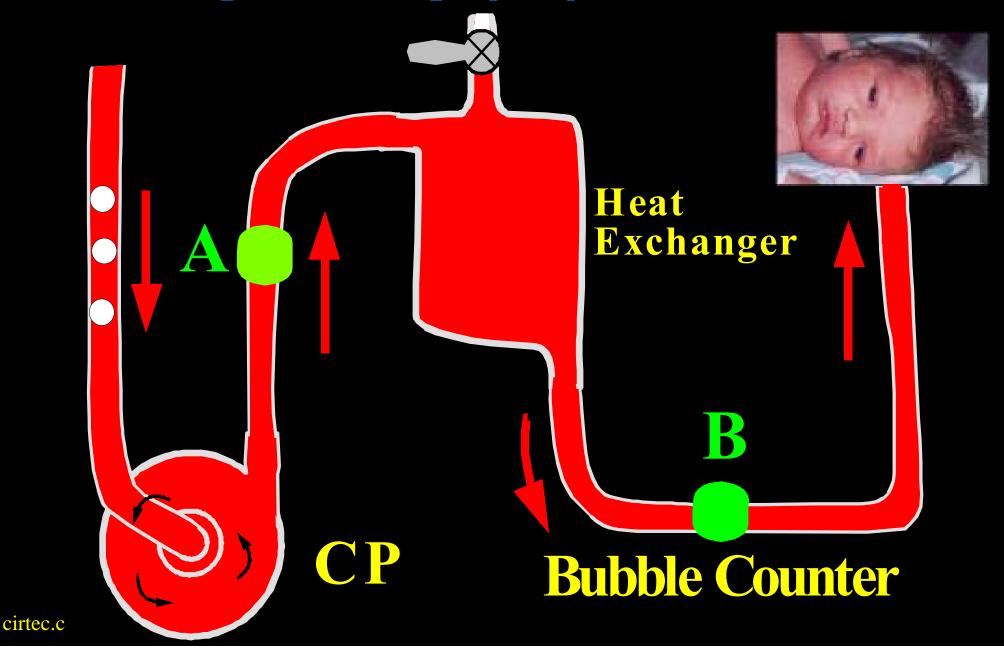


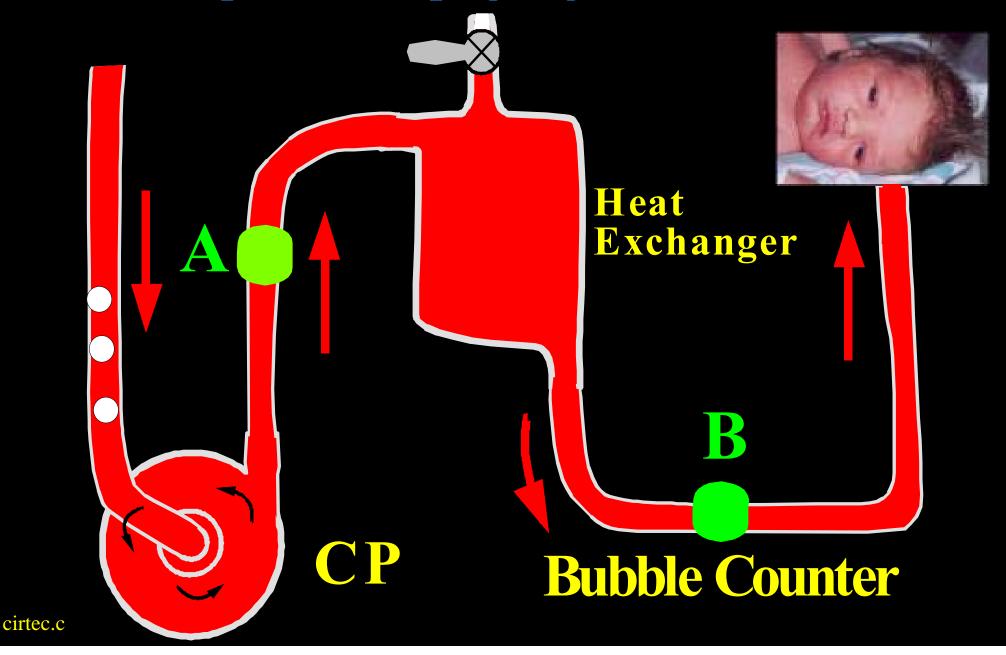


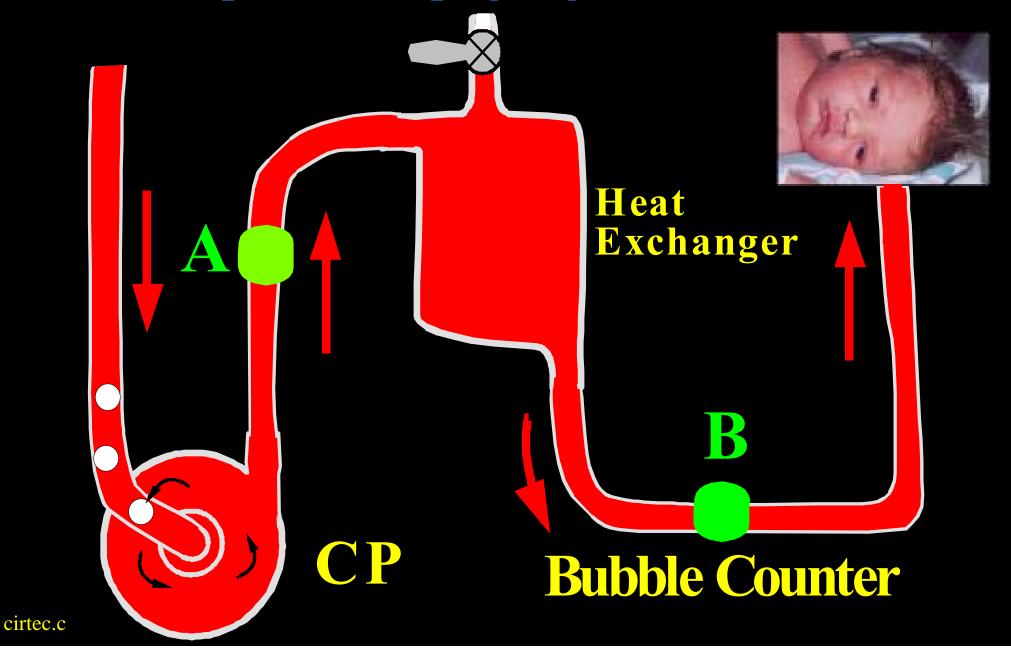


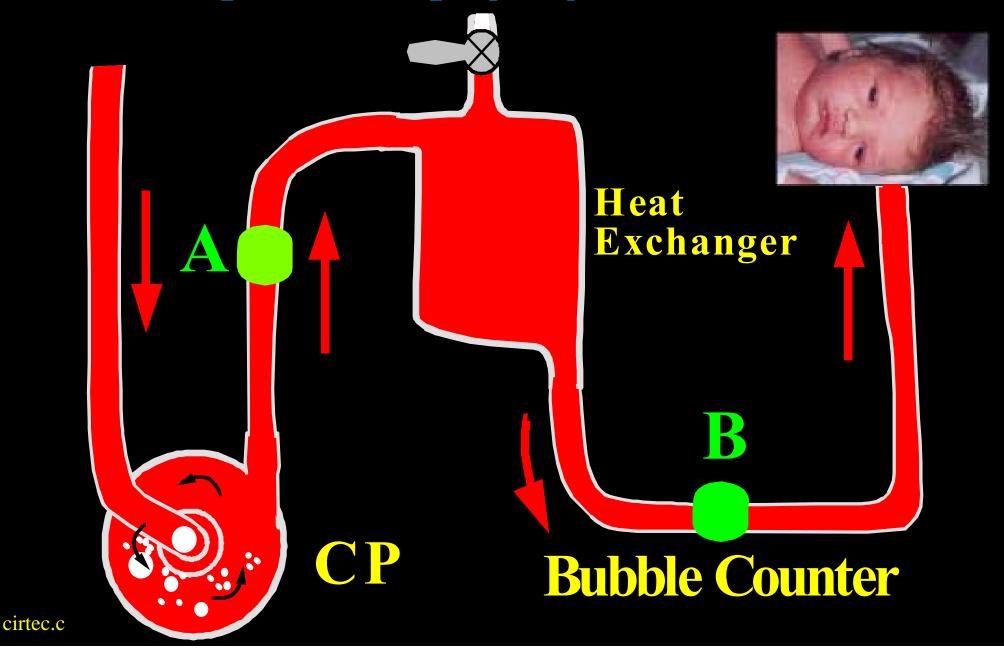


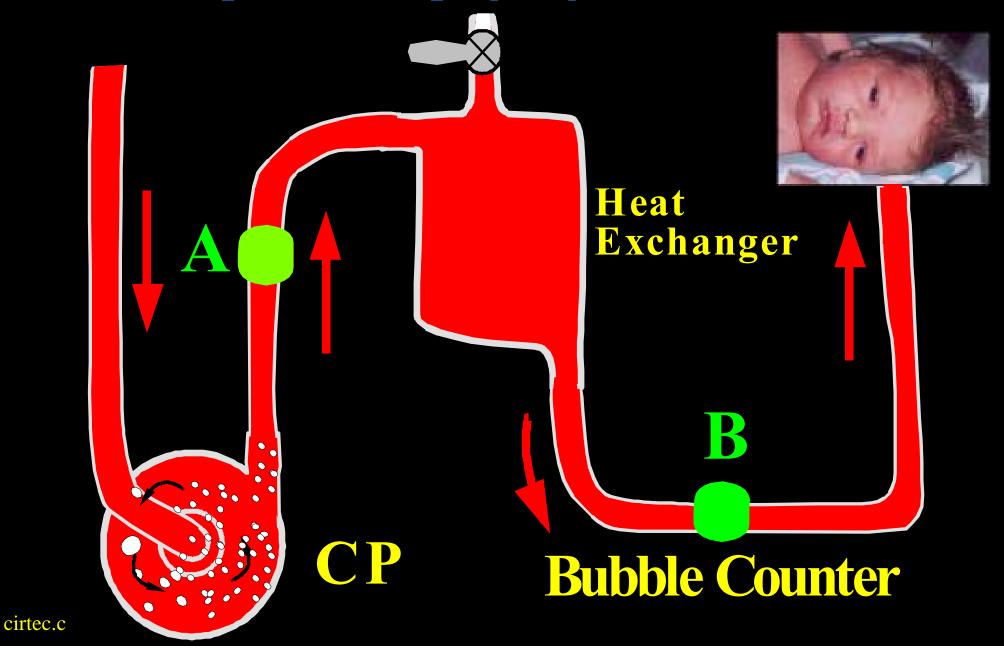


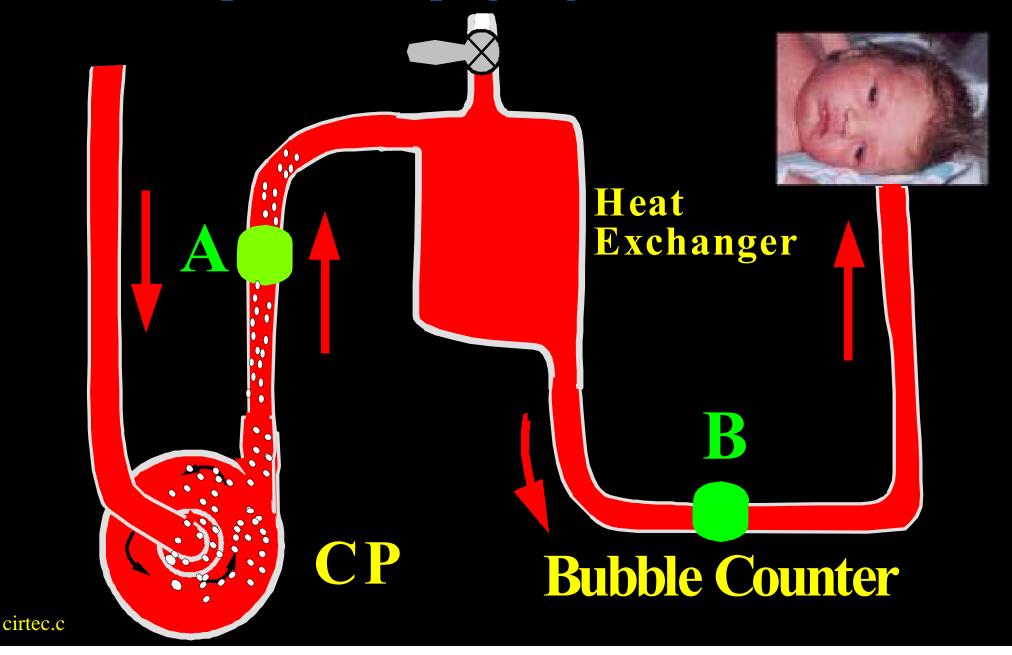


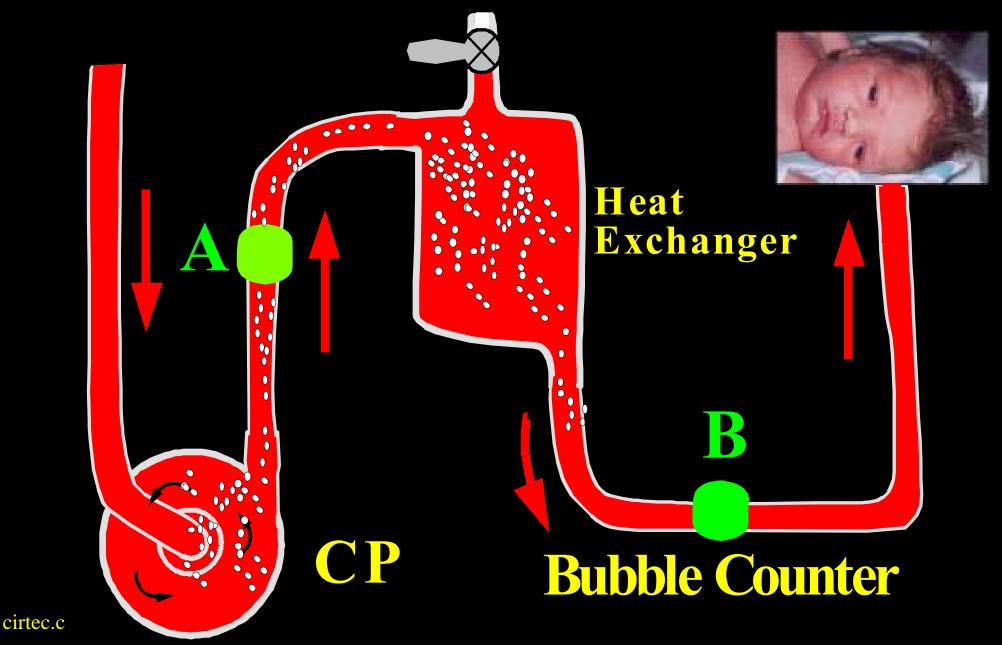




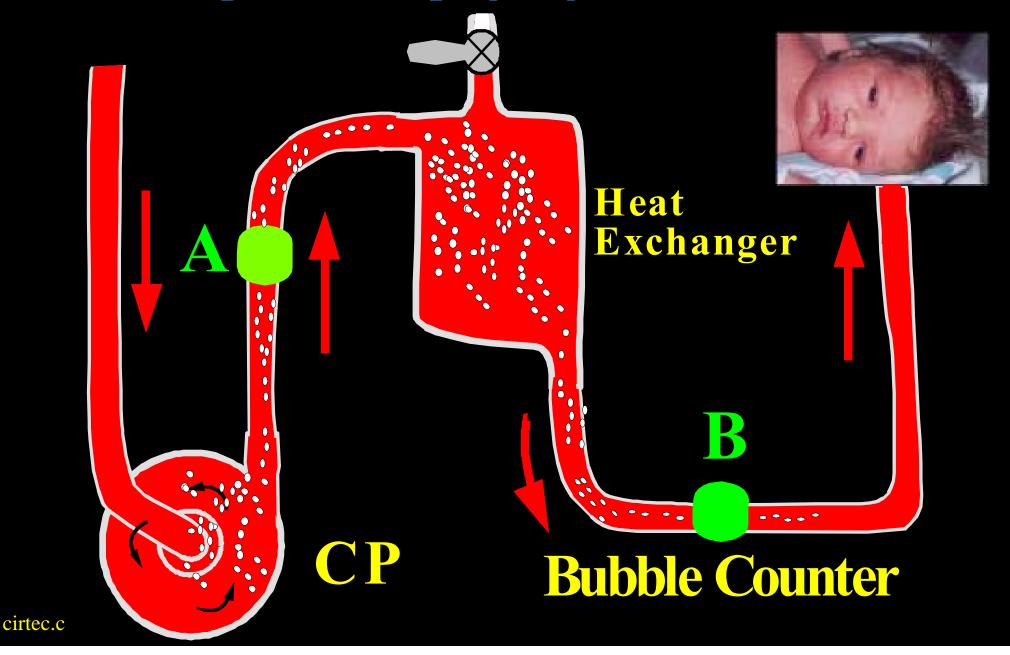




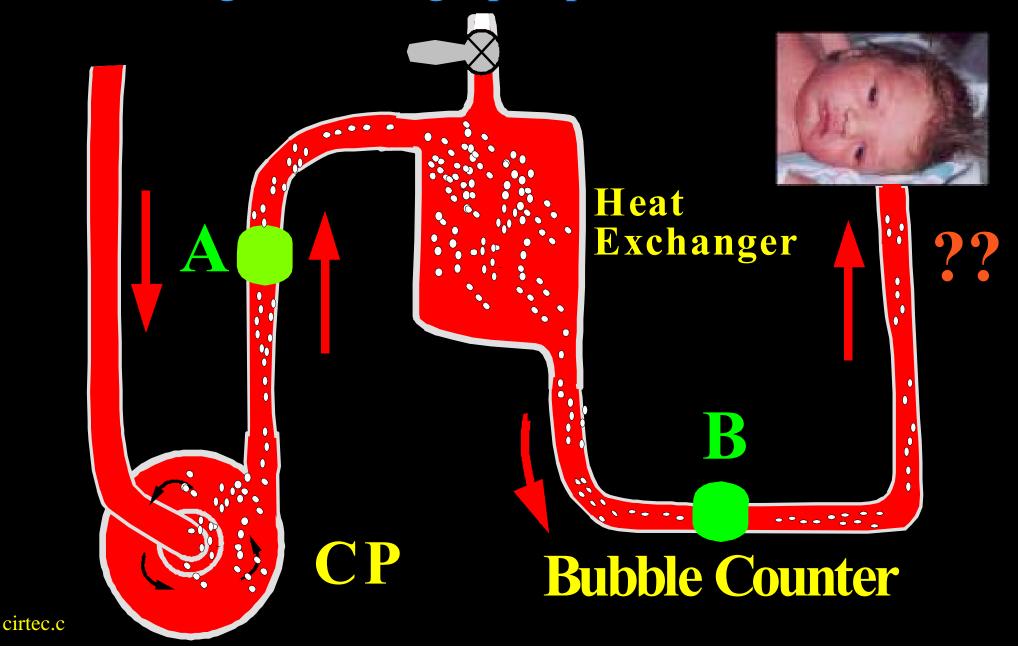


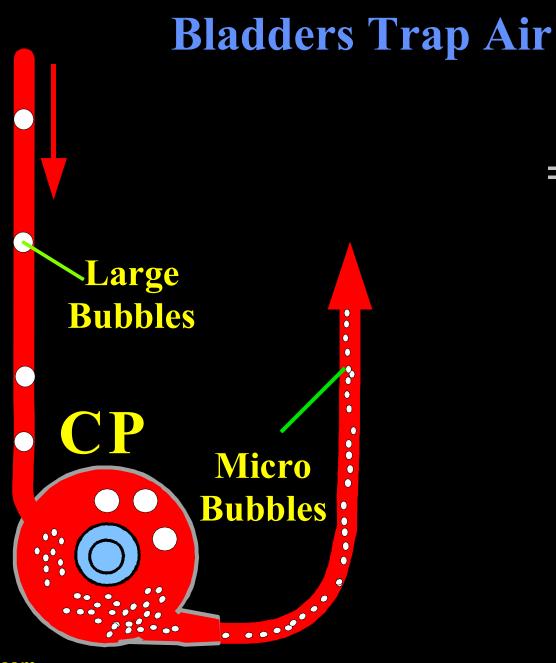


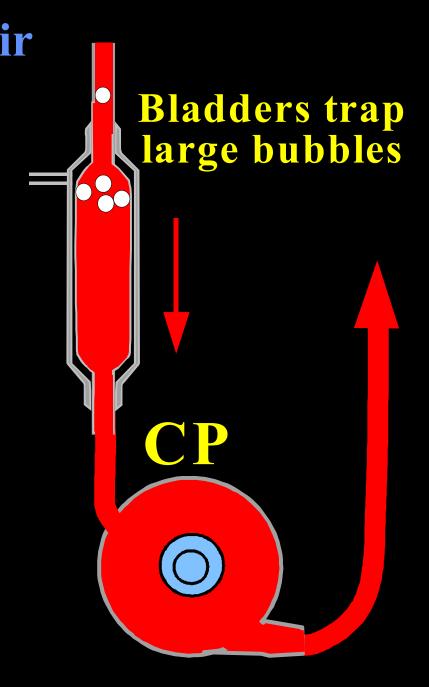
Air handling of centrifugal pumps



Air handling of centrifugal pumps

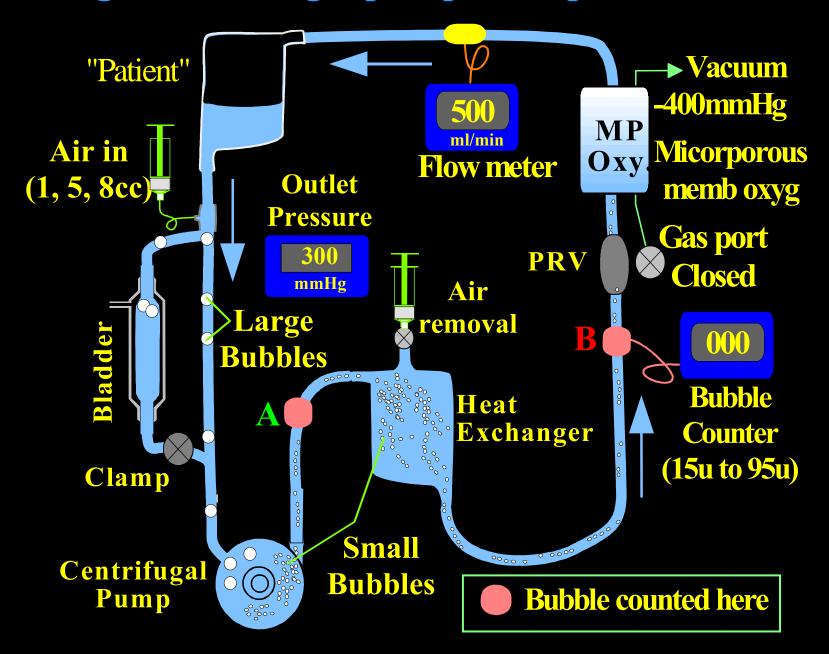




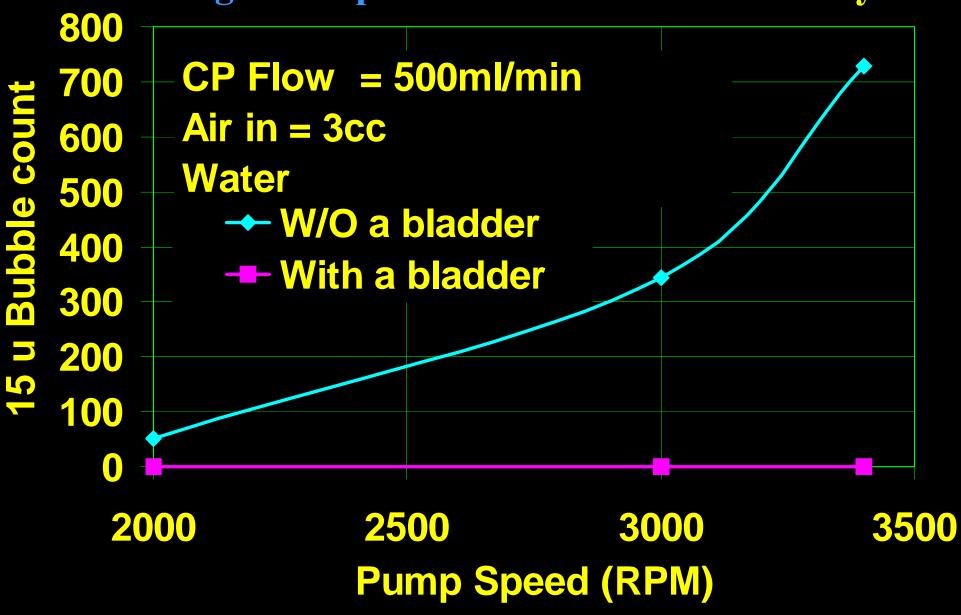


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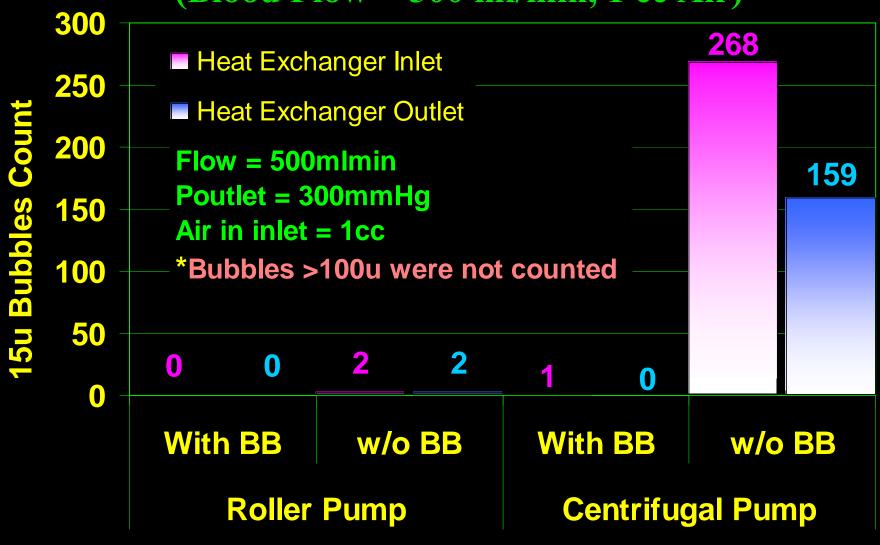
Air handling of centrifugal pumps – Experimental setup



Centrifugal Pump for ECMO – The Air Study



Centrifugal Pump for ECMO – The Air Study (Blood Flow = 500 ml/min, 1 cc Air)



Bladders Add a Safety to Centrifugal Pumps Used for ECMO

- Provide compliance that reduces rate of change in pressure and allow better pump control as a function of venous line pressure.
- Reduce the maximum negative pressure due to abrupt stoppage of venous flow.
- Eliminate negative pressure at the outlet of the pump due to abrupt stoppage of venous flow.
- Reduce microbubbles generation by the pump.

To Bladder or not to Bladder? - Costs Considerations

Avg. cost for a neonatal ECMO ~ \$100,000/wk. Peds, post-op cardiac cases, adults, etc. are much higher.

Avg. Cost of ECMO pt. - entire hospital stay \$300,000

The bladder cost is about 0.1% of the total cost.

To Bladder or not to Bladder? - Costs Considerations

Costs of post hospital care are also significant.

52% ECMO infant survivors have abnormal neuro-imaging (Bulas & Glass Semin Perinat 29:58-65 2005)

12 % have severe mental handicap (FSIQ < 70) and 37% are at risk for school failure.

(Rais-Bahrami et. al. Clin Pediatr: 39(3):145-52, 2000)

The bladder cost is less then 0.1% of the total cost.

To Bladder or not to Bladder?

Costs Considerations

Since the bladder's cost less then 1/1000 of the total cost of ECMO,

If the bladder prevents a single patient from being exposed to microbubbles or vessel damage due to excess negative pressure at the cannula

Then its cost has been justified for hundreds of patients.

Bladders placed at the pump inlet

- Dramatically reduce the maximum negative pressure at the pump inlet and at the tip of the venous cannula. Reduced vessel damage?
- Reduce pressure pulsations at the pump inlet and at the tip of the venous cannula. More Physiological?
- Provide smoother pump operation. Less clotting?
- Cleared by the FDA for that purpose.
- Standard of care reduce liability.

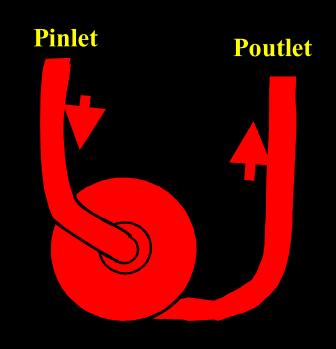
To change a circuit/procedure the user must answer to the affirmative the following:

- Is it as safe or safer then current practice?
- Is it standard of care?
- Is it supported by publications in a peer reviewed journal?
- Could it introduce other problems?
- Do we have the team with the educational background to properly evaluate the effects of the change?

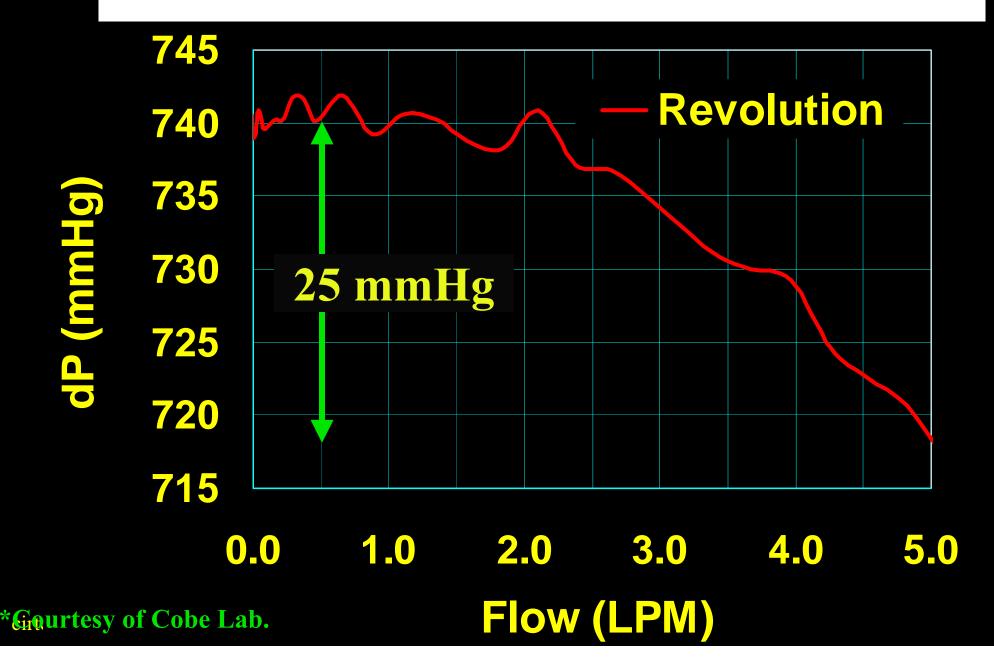
Blood damage: The Centrifugal Pump

Depends on shear stress (i.e. RPM) and exposure time.

The greater the shear and the longer the exposure time the greater the damage.



CP's Flow Characteristics*



Blood damage: The Centrifugal Pump

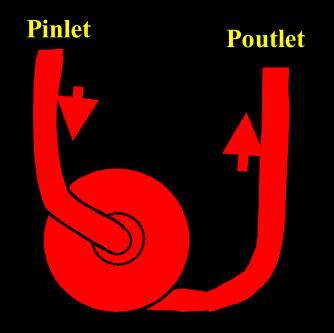
Since the line pressure in the adult and neonate circuits are similar.

And, since the pump speed varies little with flow but is mostly dependent on line pressure.

Then, we can conclude that the shear stress within the pump for neonates approximates that for adults.

Any difference in blood damage between adults and neonates flow conditions is due to differences in exposure times to that shear.

Blood damage by CPs



Patient	Pout mmHg	Flow LPM	Time sec
Adult	<i>250</i>	5.0	0.6
Neonate	<i>250</i>	0.5	6.0

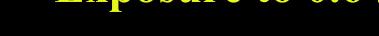
For a CP with a prime volume of 50 ml, the residence time at 5.0 LPM is 0.6 sec. At 0.5 LPM it is 10 times longer or 6.0 sec.

The finger damage test



_ Little or no damage.

Exposure to 0.6 sec



The finger damage test



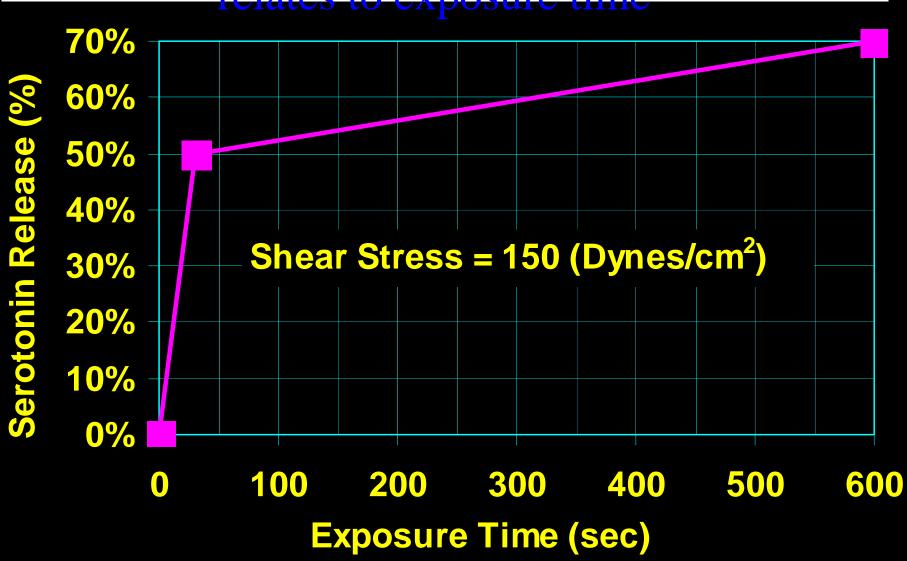


Major damage





Serotonin released from sheared platelets relates to exposure time*

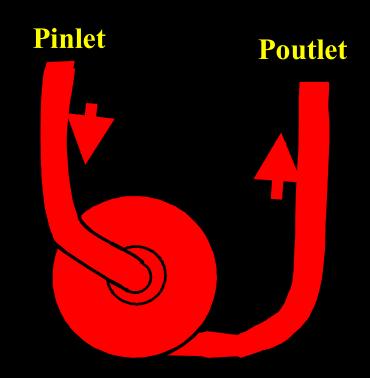


*drivouvemet.al. Trans. ASAIO 21:35, '75

Blood damage: Comparing RP to CP

Hemolysis: Shear stress (i.e. RPM) Exposure time.

RPM = f (pressure) Exposure time = f (1/Flow)



Shear x Time \cong Pressure x (1/Flow)

The effects of pressure and flow on hemolysis caused by Bio-Medicus centrifugal pumps and roller pumps. Guidelines for choosing a blood pump.

Tamari Y, Lee-Sensiba K, Leonard EF, Parnell V, Tortolani AJ. J Thorac Cardiovasc Surg. 1993 Dec;106(6):997-1007.

Guidelines for choosing a blood pump: RP v. CP



0.0 0.2 0.4 0.6 0.8 1.0 1.2 1.4 1.6 1.8 2.0 Pressure/Flow (mmHg/(ml/min))

Guidelines for choosing a blood pump: RP v. CP

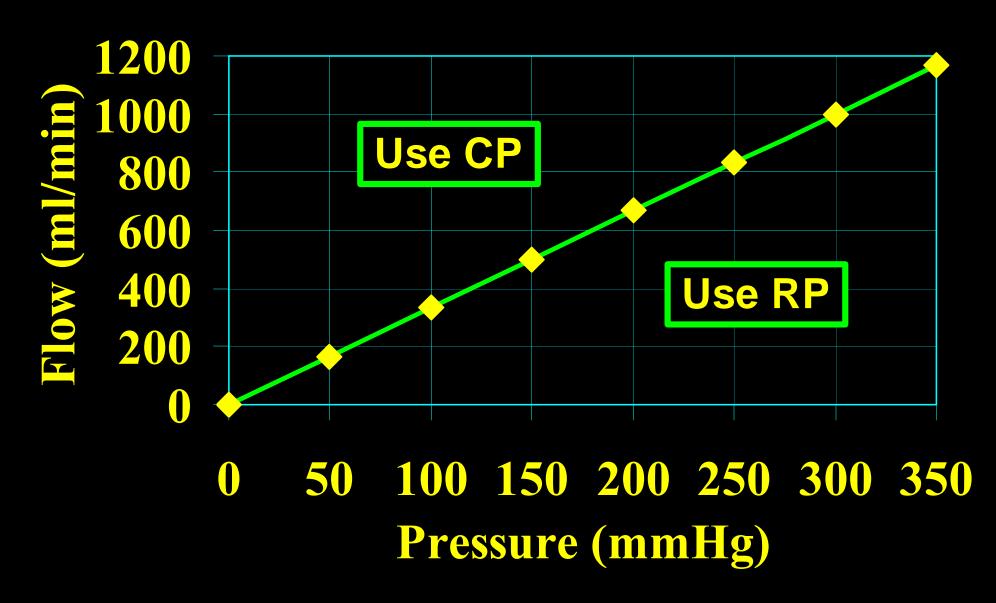
Hemolysis for the Biopump is higher than that of the roller pump when the ratio of the pressure divided by the flow is less than 0.35

When:

Pressure(mmHg)/Flow(ml/min) > 0.35

use the roller pump.

Hemolysis – Choosing between RP and CP



Hemolysis – Choosing between RP and CP

It is important to note that in later studies, when the RP was set nonocclusively, the RP was always less hemolytic than the CP*.

*A dynamic method for setting roller pumps nonocclusively reduces hemolysis and predicts retrograde flow.

Tamari Y, Lee-Sensiba K, Leonard EF, Tortolani AJ. ASAIO J. 1997 Jan-Feb;43(1):39-52.

Questions?

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